

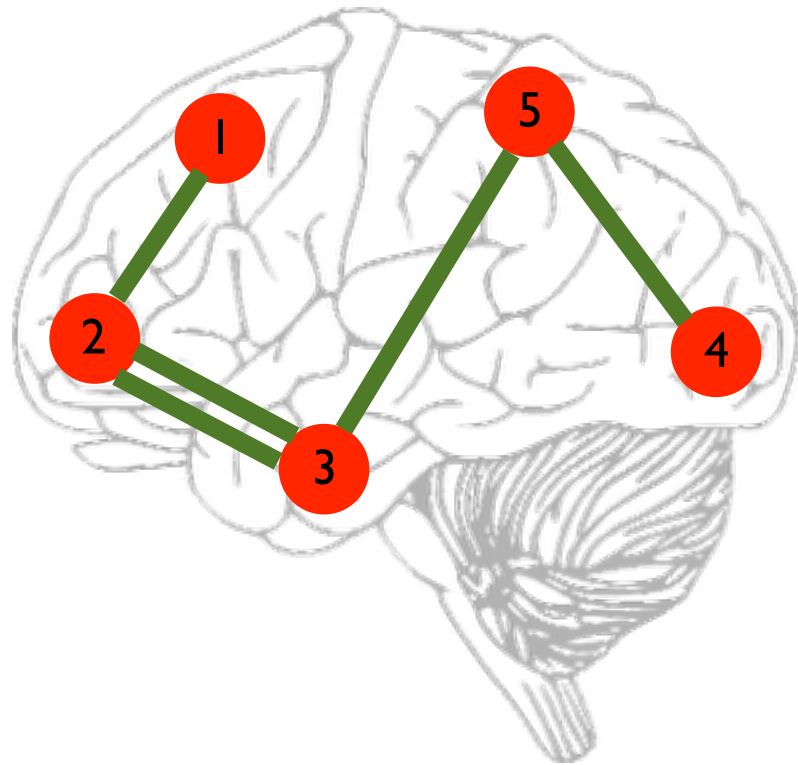
# From Static to Fast Transient Dynamic Brain Networks

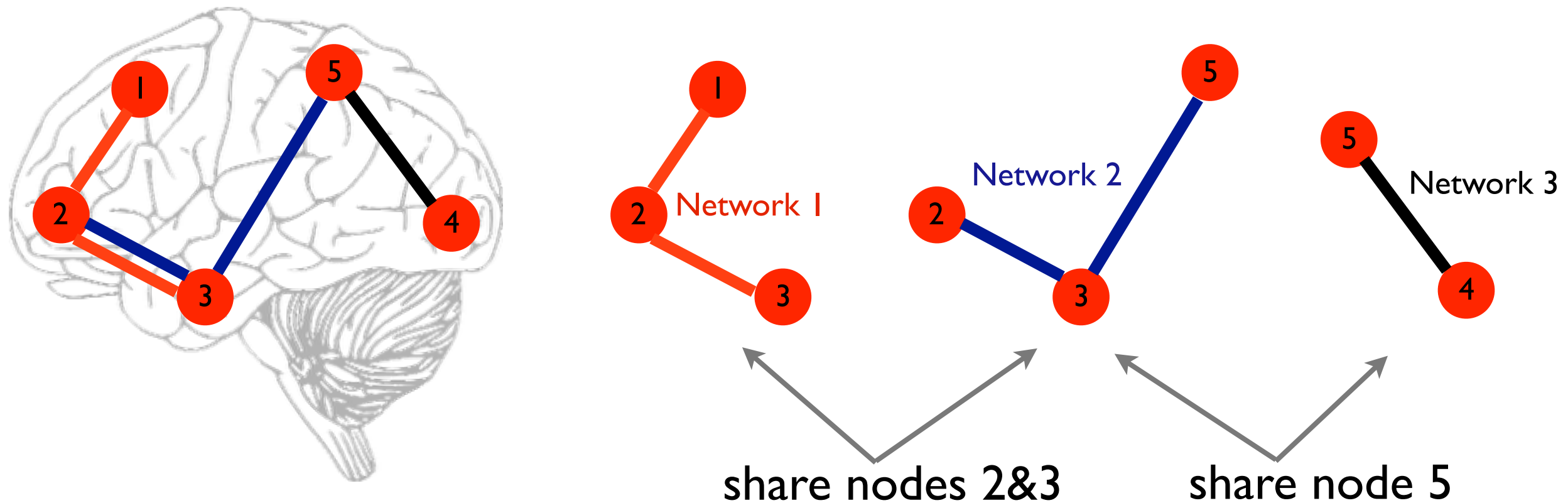
*Diego Vidaurre*  
Department of Psychiatry  
*University of Oxford*



Oxford centre for Human Brain Activity

# Resting state network





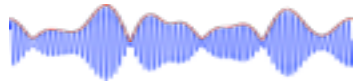
Network 1, 2 and 3 have distinct spatial and temporal characteristics that could not have been found in a static analysis

- What is happening at **faster** time-scales?
- What are the specific temporal interactions, or network dynamics?
- How activity organises temporally and spatially in rest, and how connectivity is modulated in task

Can we use MEG to answer these questions?

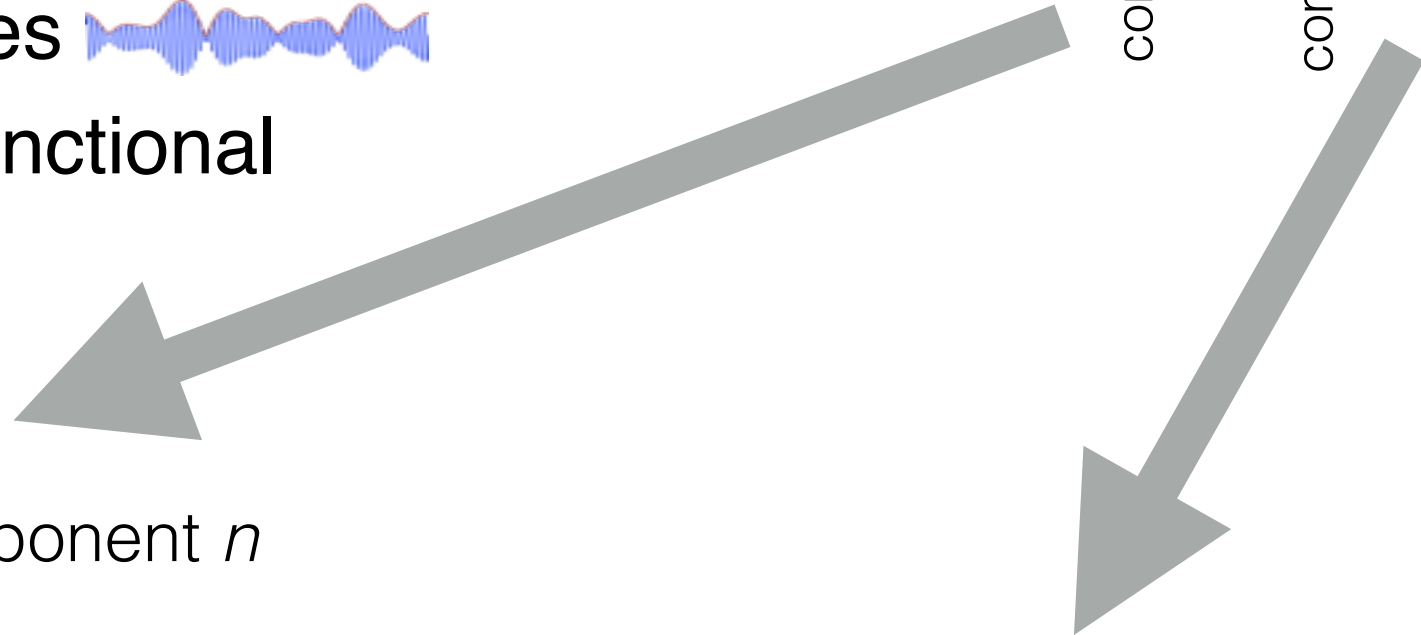


## Temporal Independent Component Analysis

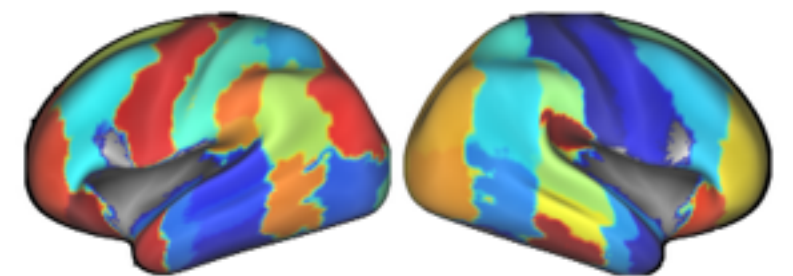
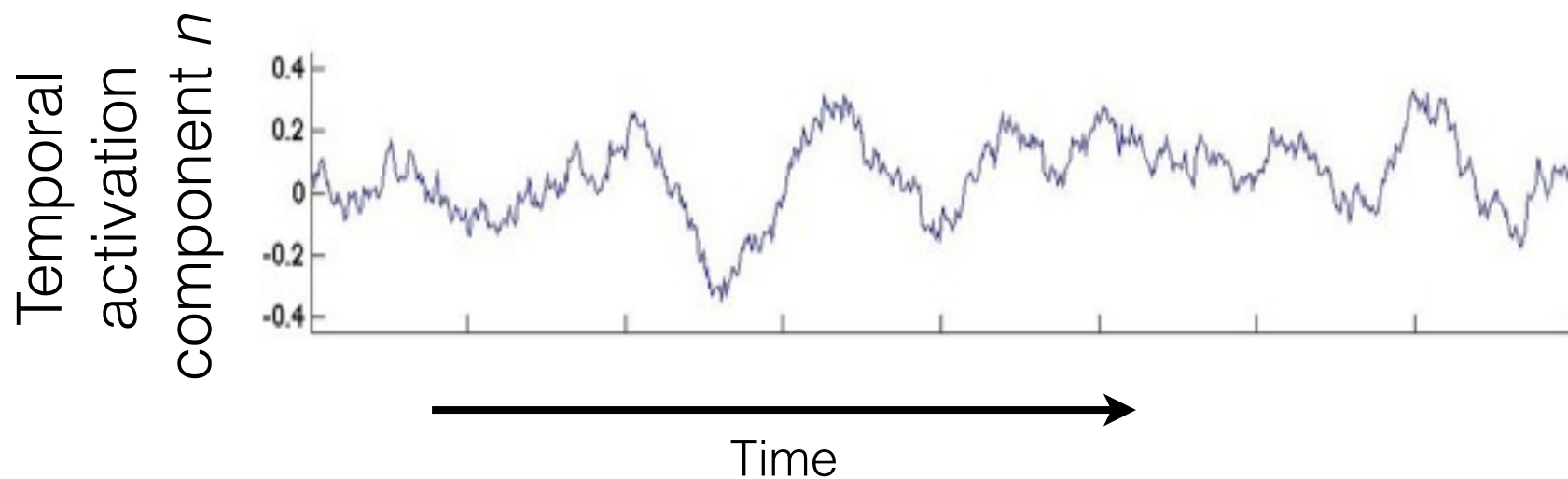
- Activation pattern or components (A)
- Component time courses (S)
- Specified on power time series 
- Components do not reflect functional connectivity

$$X = S A$$

time  
×  
regions
time  
×  
components
components  
×  
regions



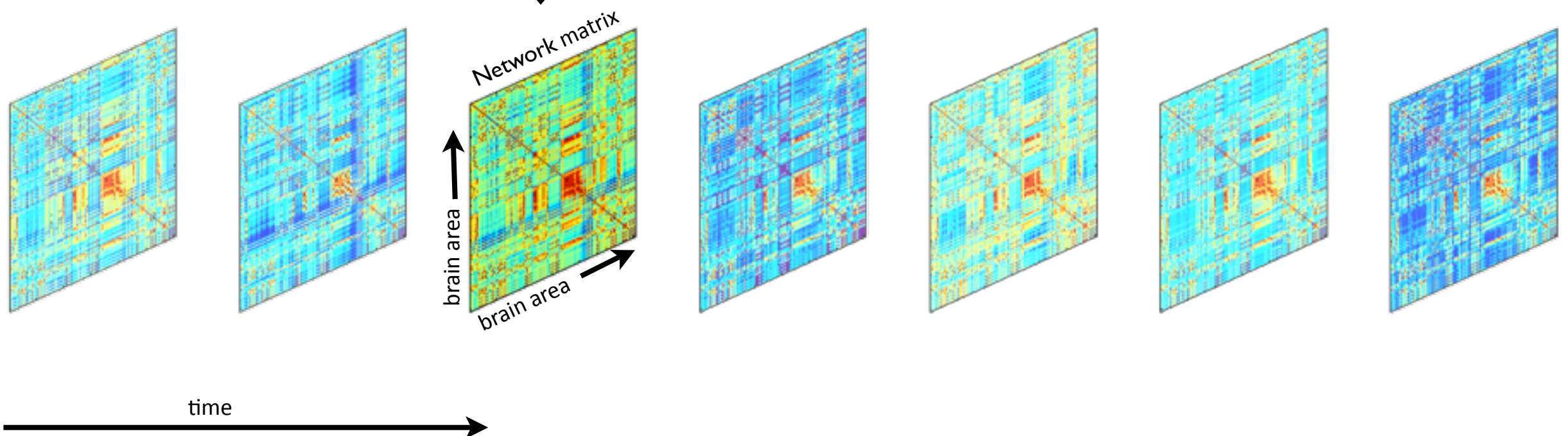
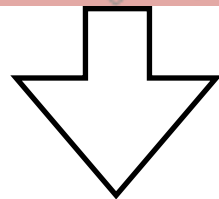
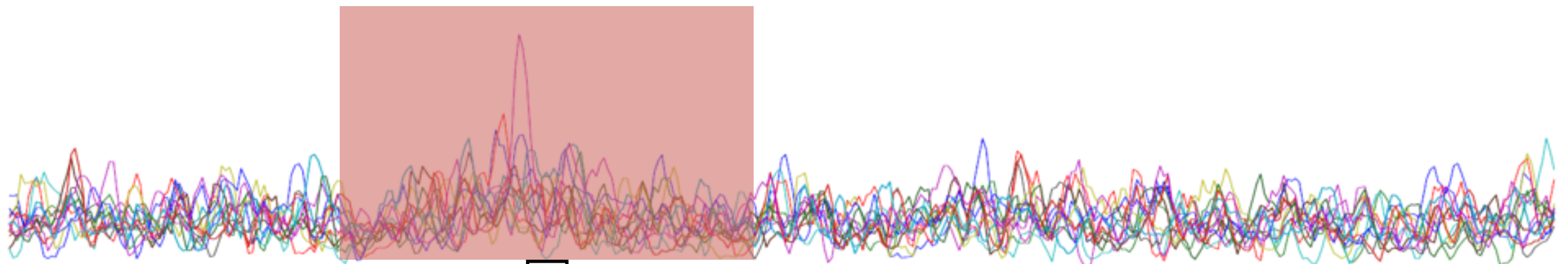
Spatial activation component  $n$



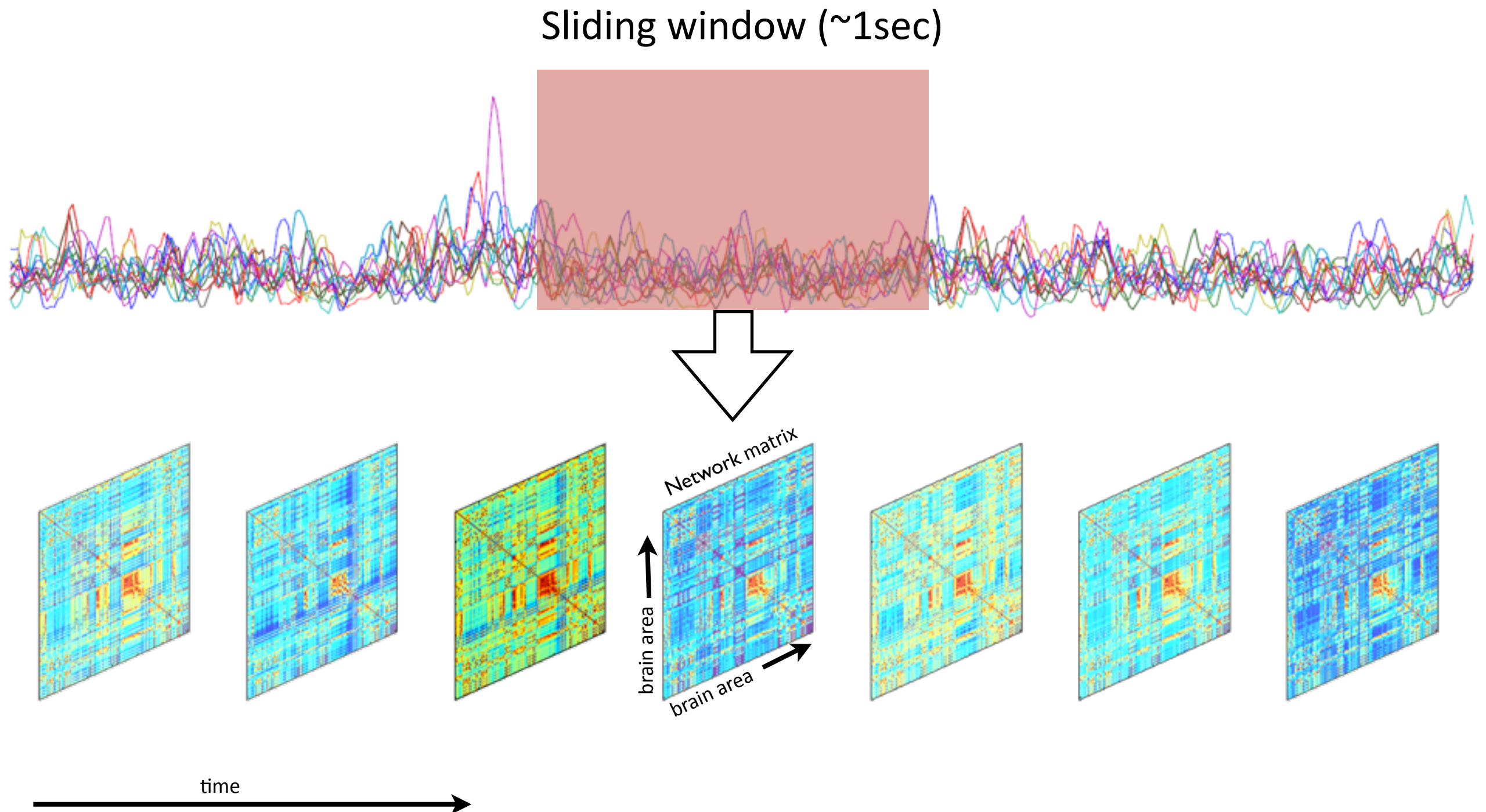


Compute **sliding window** correlation network matrices

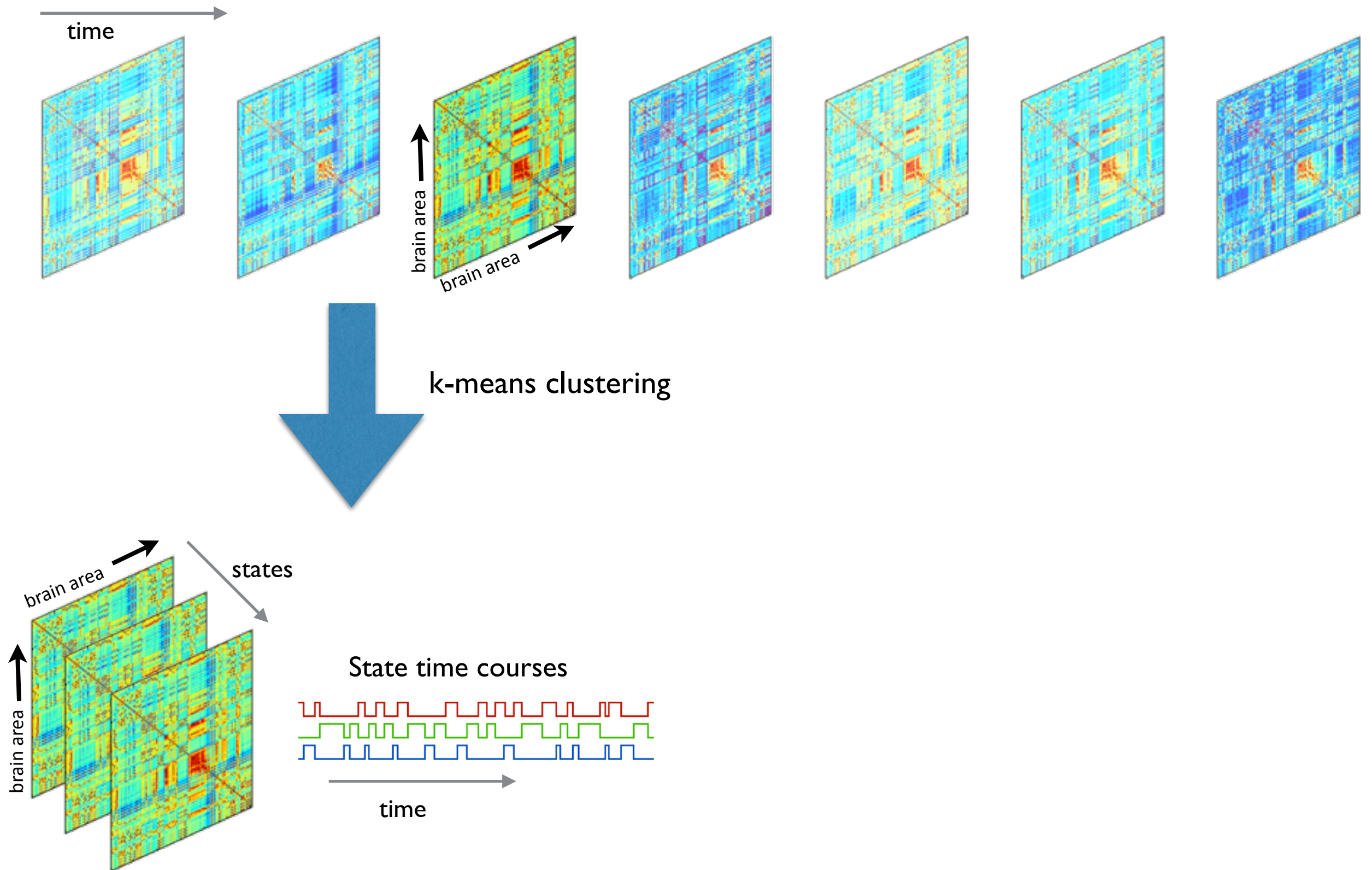
Sliding window (~1sec)



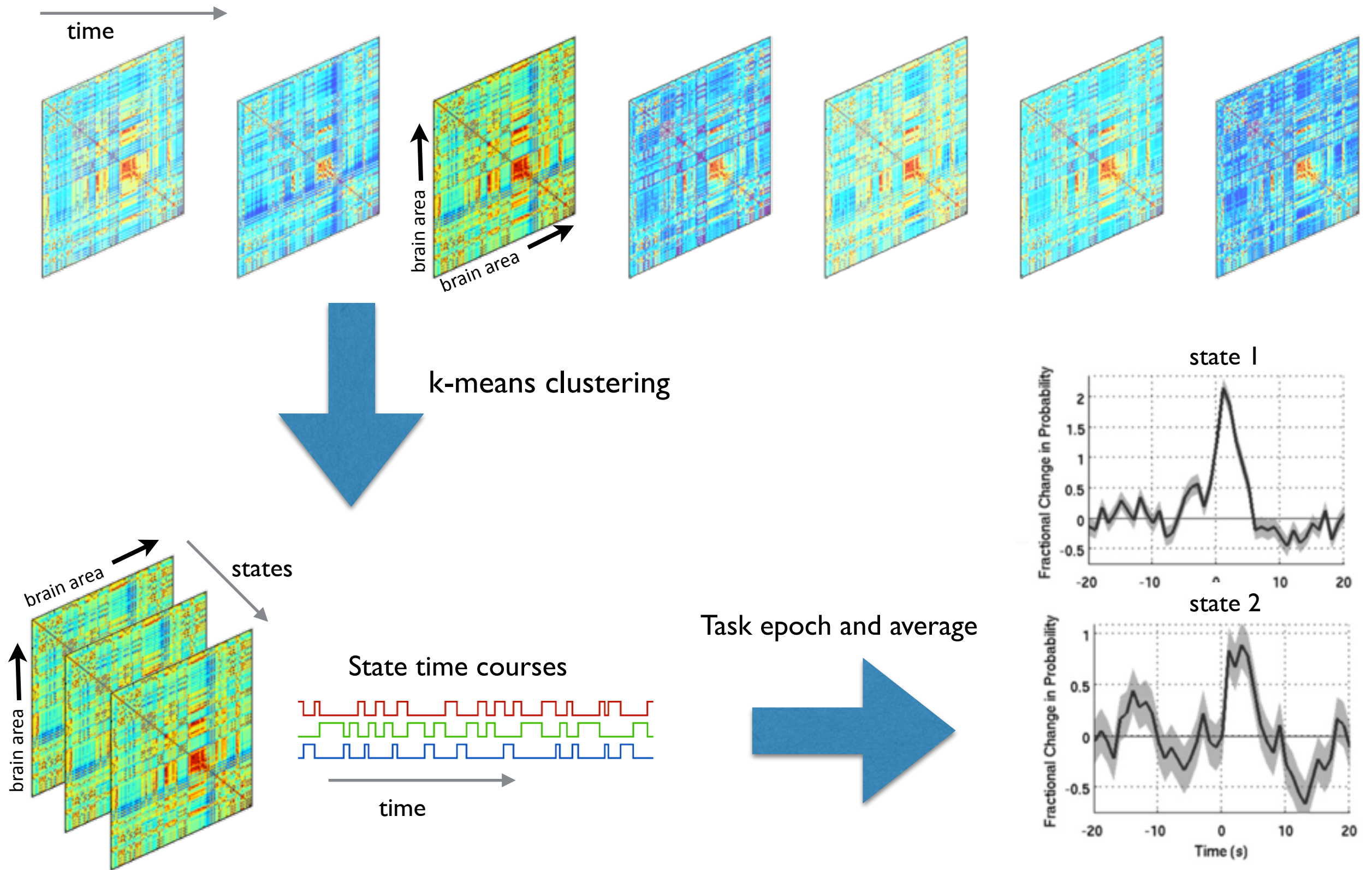
Compute **sliding window** correlation network matrices











## Issues:

### How to choose the width of the window?

- too short - unstable, unreliable estimation
- too long - misses quick changes

### Inefficient use of the data

- No matter how much data we have, each estimation is based on a small portion of the data



Can sliding-window correlations reveal dynamic functional connectivity in resting-state fMRI?

R. Hindriks<sup>a,\*</sup>, M.H. Adhikari<sup>a</sup>, Y. Murayama<sup>d</sup>, M. Ganzetti<sup>b,c</sup>, D. Mantini<sup>b,c</sup>, N.K. Logothetis<sup>d</sup>, G. Deco<sup>a,e</sup>

<sup>a</sup> Center for Brain and Cognition, Computational Neuroscience Group, Department of Information and Communication Technologies, Universitat Pompeu Fabra, Barcelona, Spain

<sup>b</sup> Department of Health Sciences and Technology, ETH Zurich, Switzerland

<sup>c</sup> Department of Experimental Psychology, University of Oxford, United Kingdom

<sup>d</sup> Department of Physiology of Cognitive Processes, Max Planck Institute for Biological Cybernetics, Tübingen, Germany

<sup>e</sup> Institut Català de Recerca i Estudis Avançats (ICREA), Universitat Pompeu Fabra, Barcelona, Spain

ORIGINAL ARTICLE

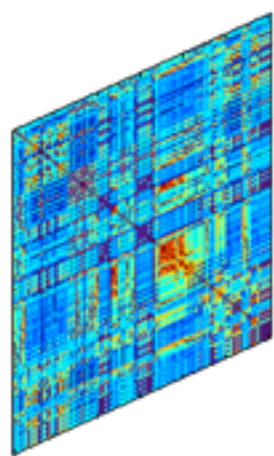
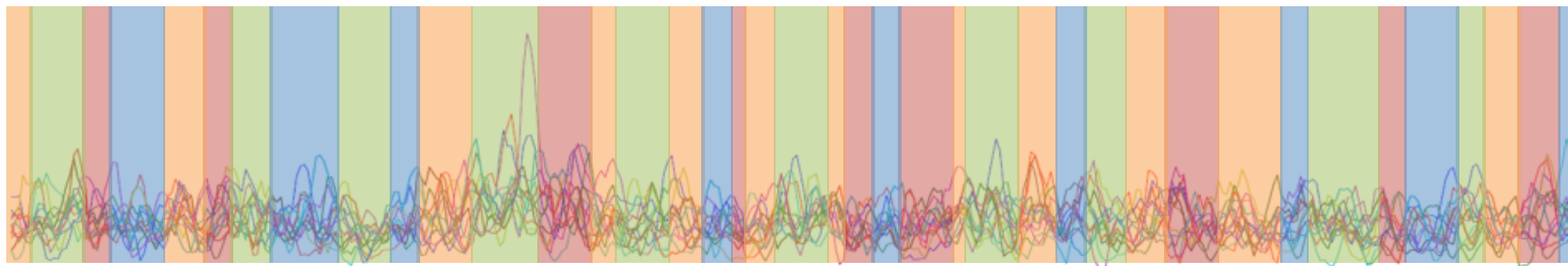
Cerebral CORTEX

### On the Stability of BOLD fMRI Correlations

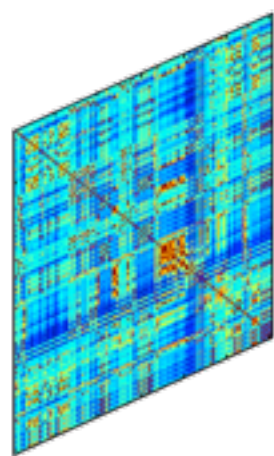
Timothy O. Laumann<sup>1</sup>, Abraham Z. Snyder<sup>1,2</sup>, Anish Mitra<sup>2</sup>, Evan M. Gordon<sup>3,4</sup>, Caterina Gratton<sup>1</sup>, Babatunde Adeyemo<sup>1</sup>, Adrian W. Gilmore<sup>5</sup>, Steven M. Nelson<sup>3,4</sup>, Jeff J. Berg<sup>5</sup>, Deanna J. Greene<sup>2,6</sup>, John E. McCarthy<sup>7</sup>, Enzo Tagliazucchi<sup>8,9</sup>, Helmut Laufs<sup>9,10</sup>, Bradley L. Schlaggar<sup>1,2,6,11,12</sup>, Nico U. F. Dosenbach<sup>1</sup>, and Steven E. Petersen<sup>1,2,5,12</sup>



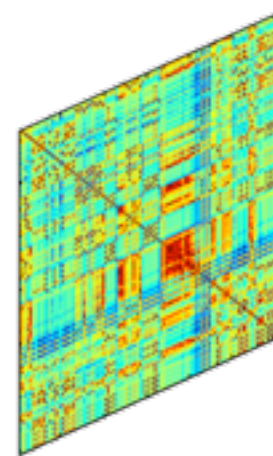
Instead pool data over disjoint time periods:



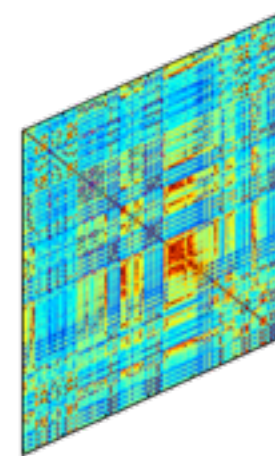
**State 1**



**State 2**



**State 3**



**State 4**

## Fundamental assumptions

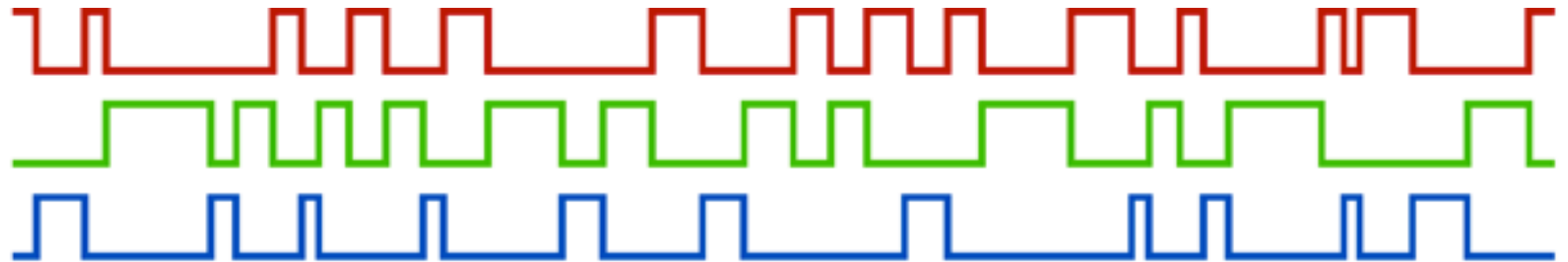
- **One state is assumed at a time**  
although we effectively estimate the probability of each state being active at each time point  $t$
- **Which state is active at time  $t$  depends on which state was active at time point  $t-1$**   
which means that the influence of the past decreases exponentially

## Benefits

- We do not need to specify the window length
- We make an efficient use of the data
- We can access the fastest time scales



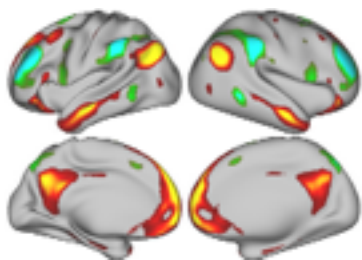
State time courses:  
**When**



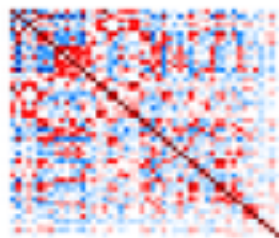
State probability distribution  
(one for each state):

**What**

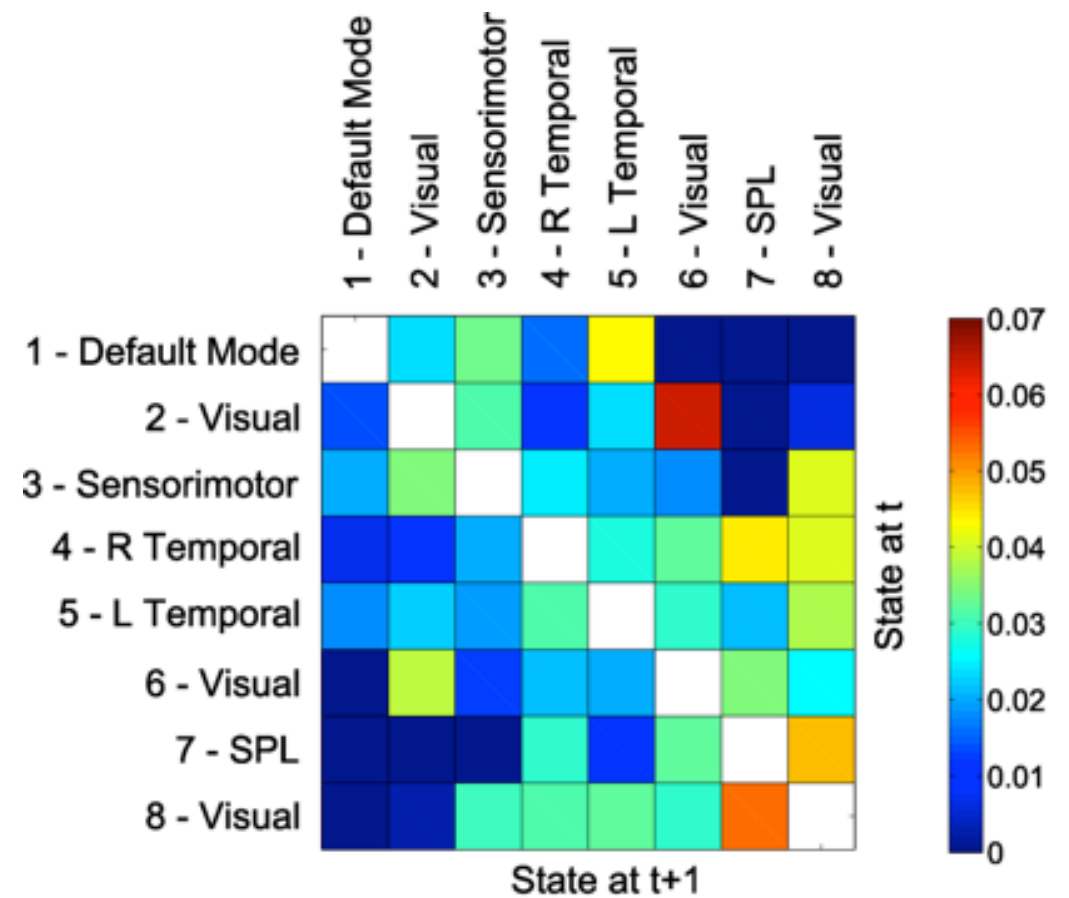
Mean activation



Functional connectivity

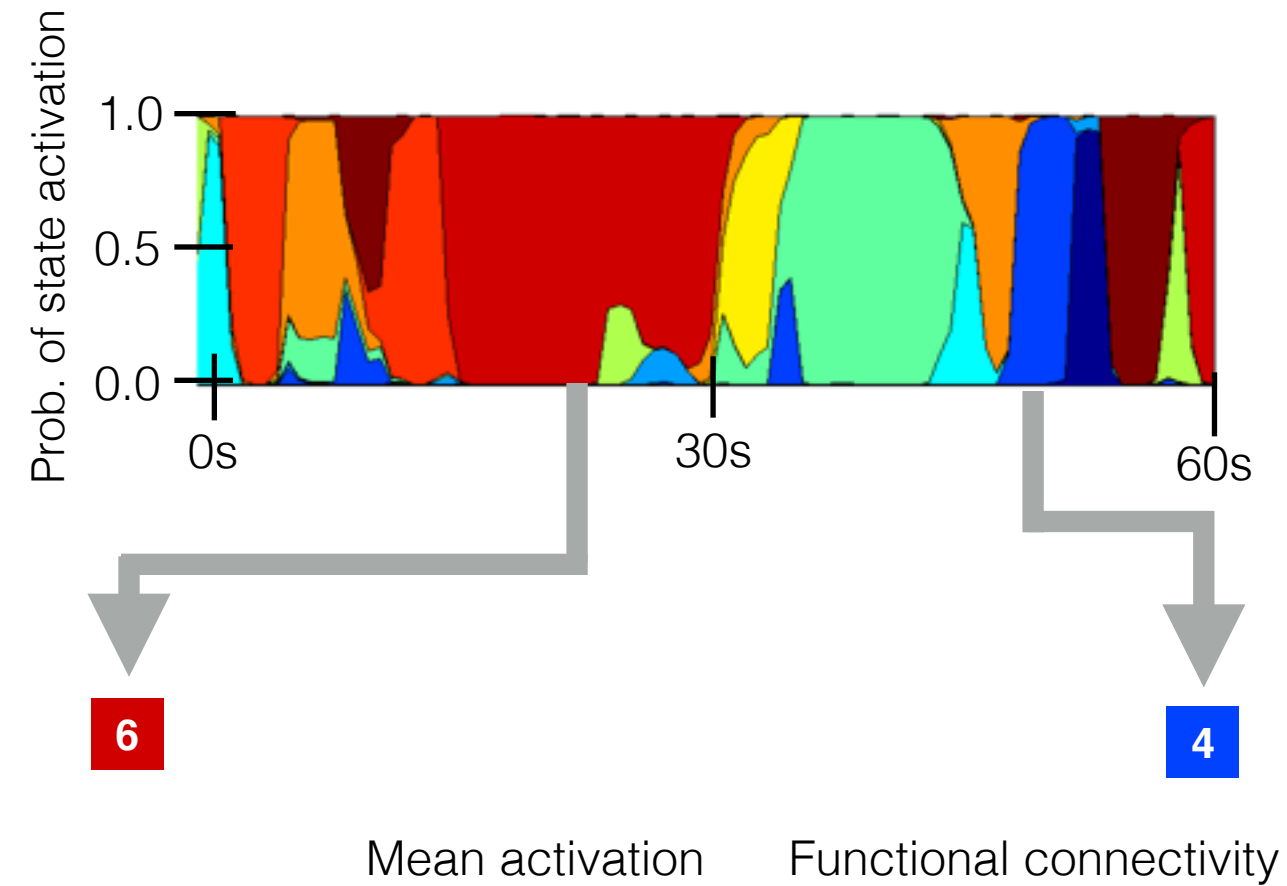


*Different classes of probability distributions adapt to different classes of data  
this is a user choice*



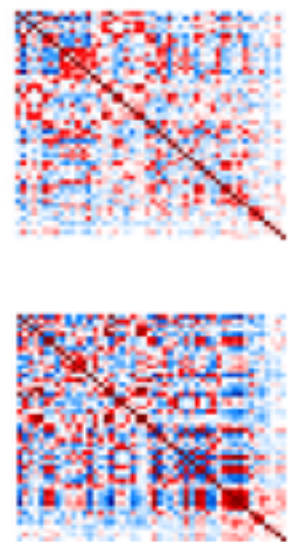
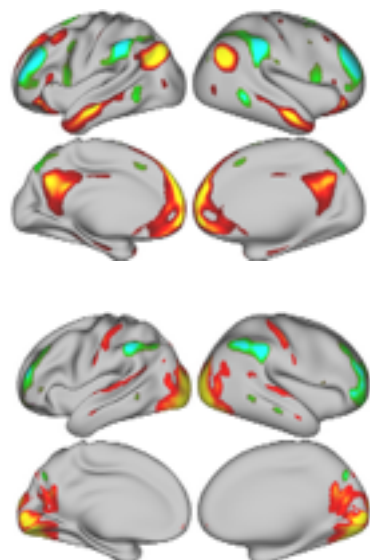
Transition probability matrix

## In rest

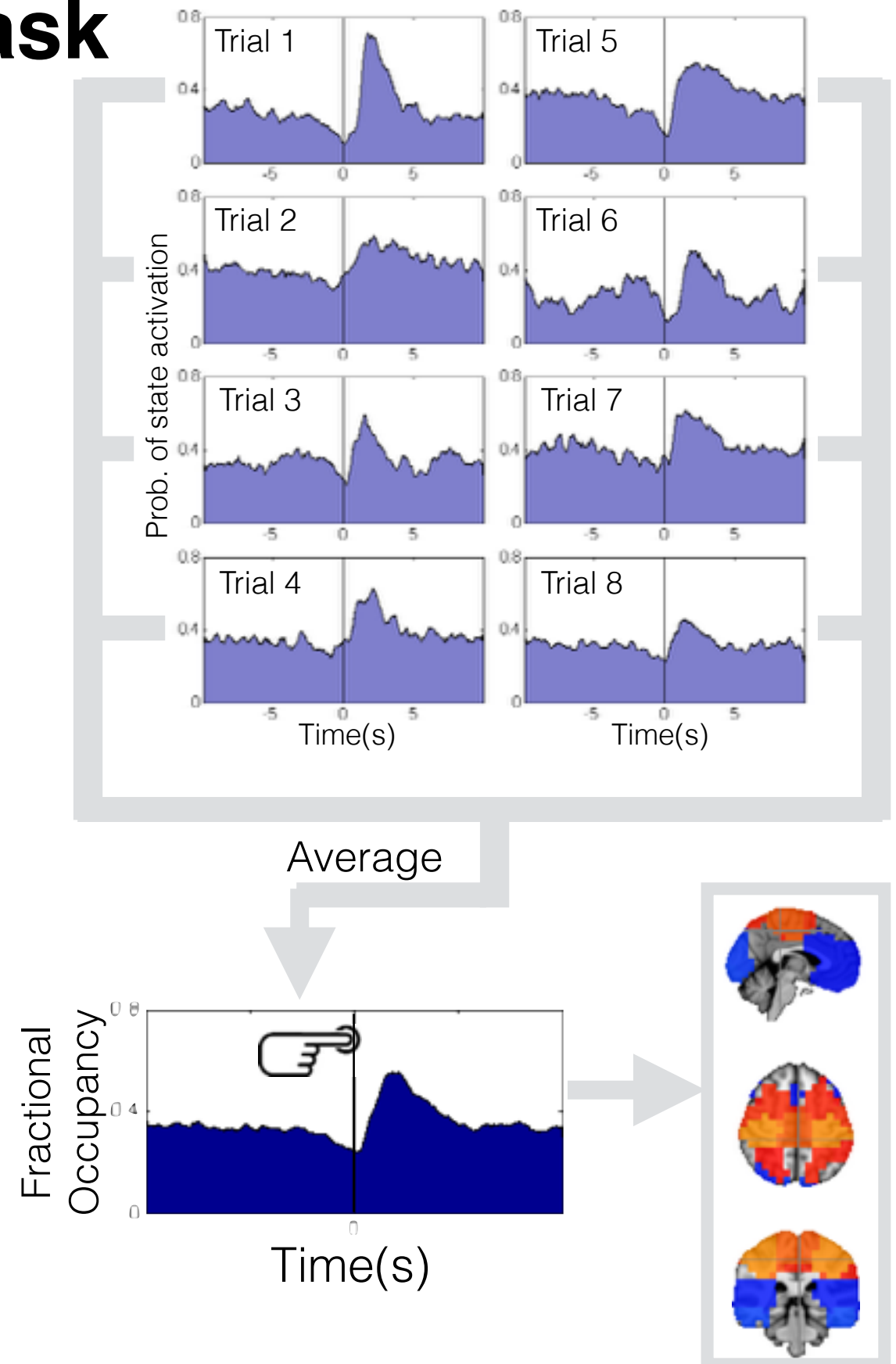


**6**  
DMN

**4**  
Visual network



## In task



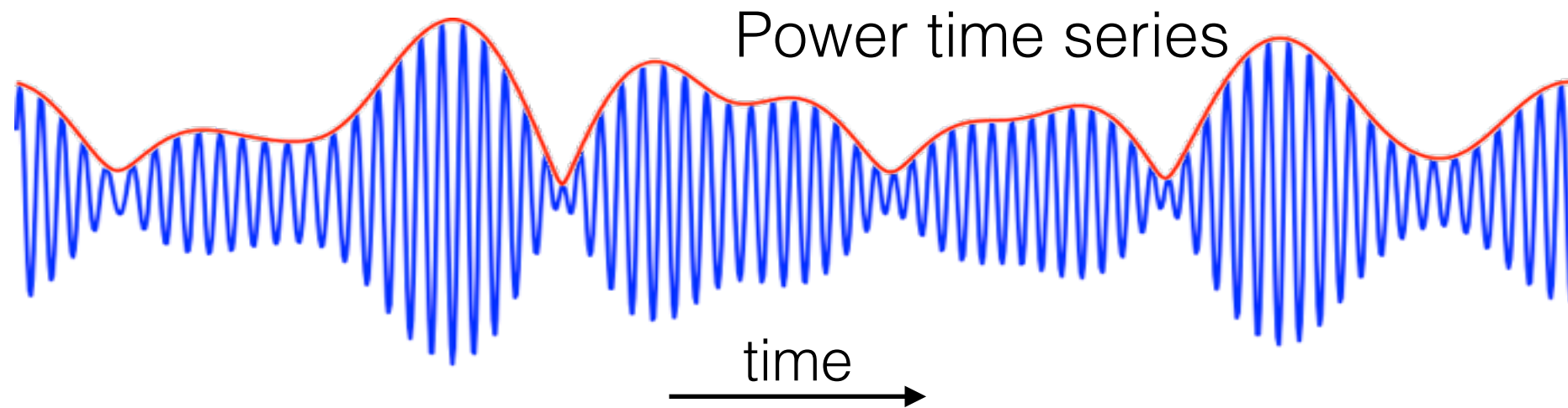
**At the group level**



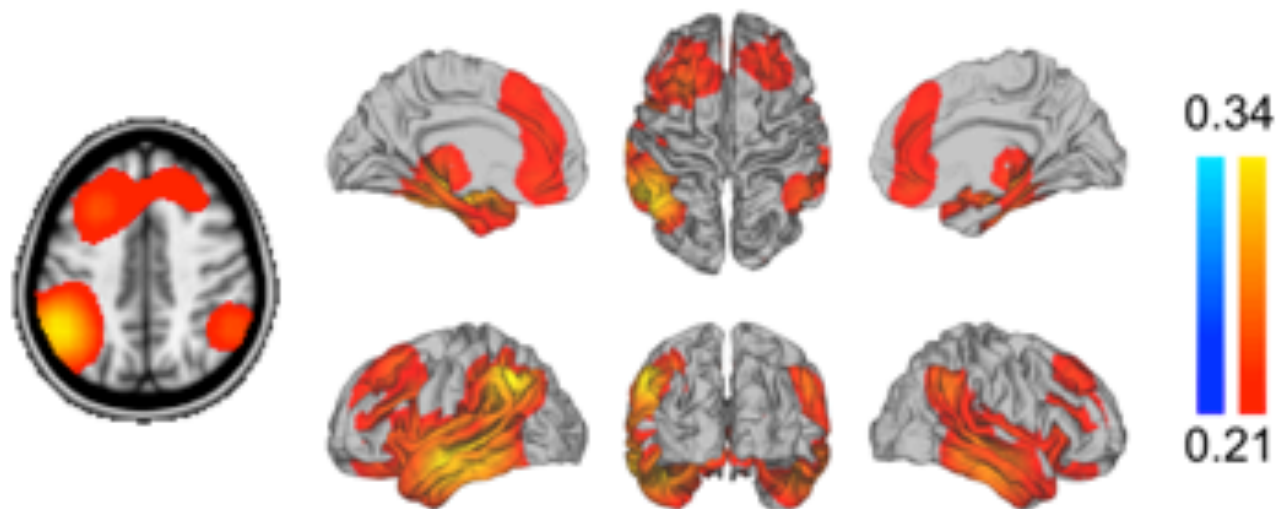
**At the subject level**



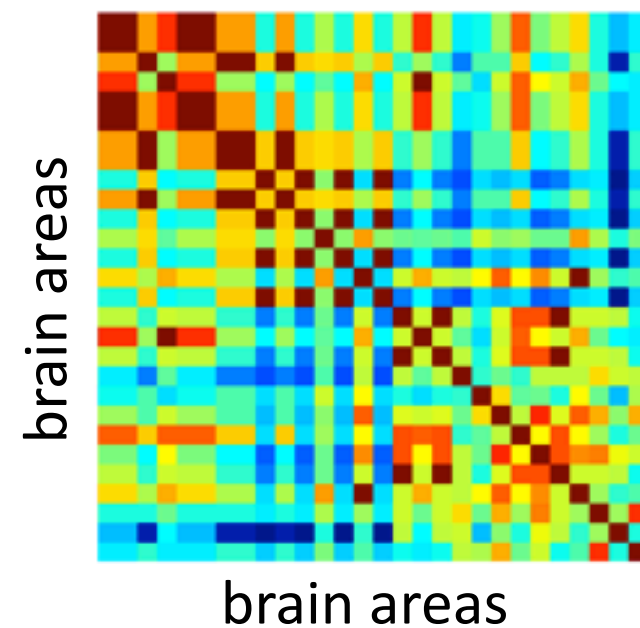
What is a brain state? A Gaussian distribution  $\mathcal{N}(\mu, \Sigma)$



Mean activation  $\mu$



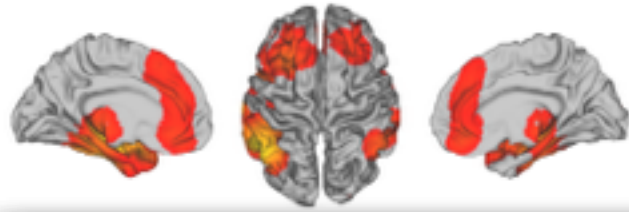
Network matrix  $\Sigma$   
(power correlation)



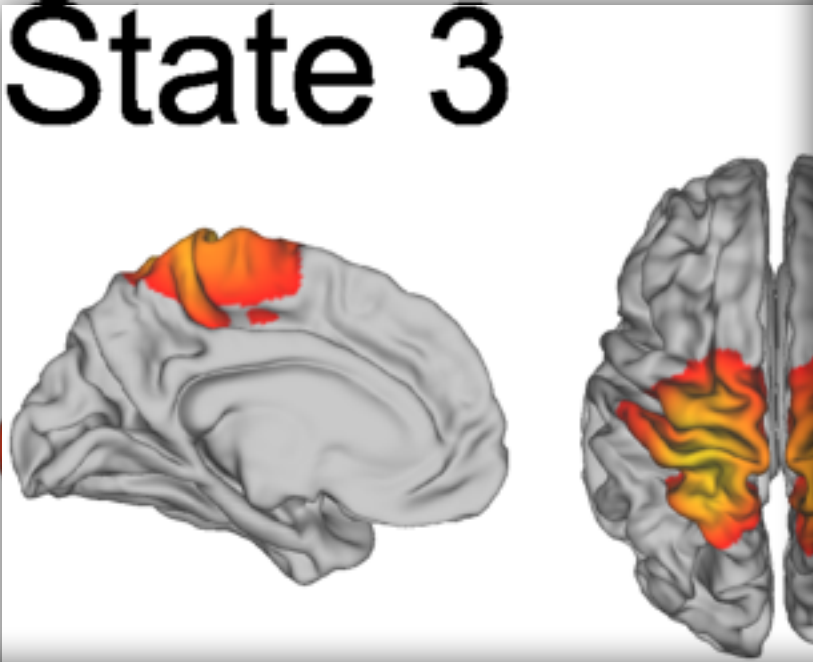


# HMM-Gaussian

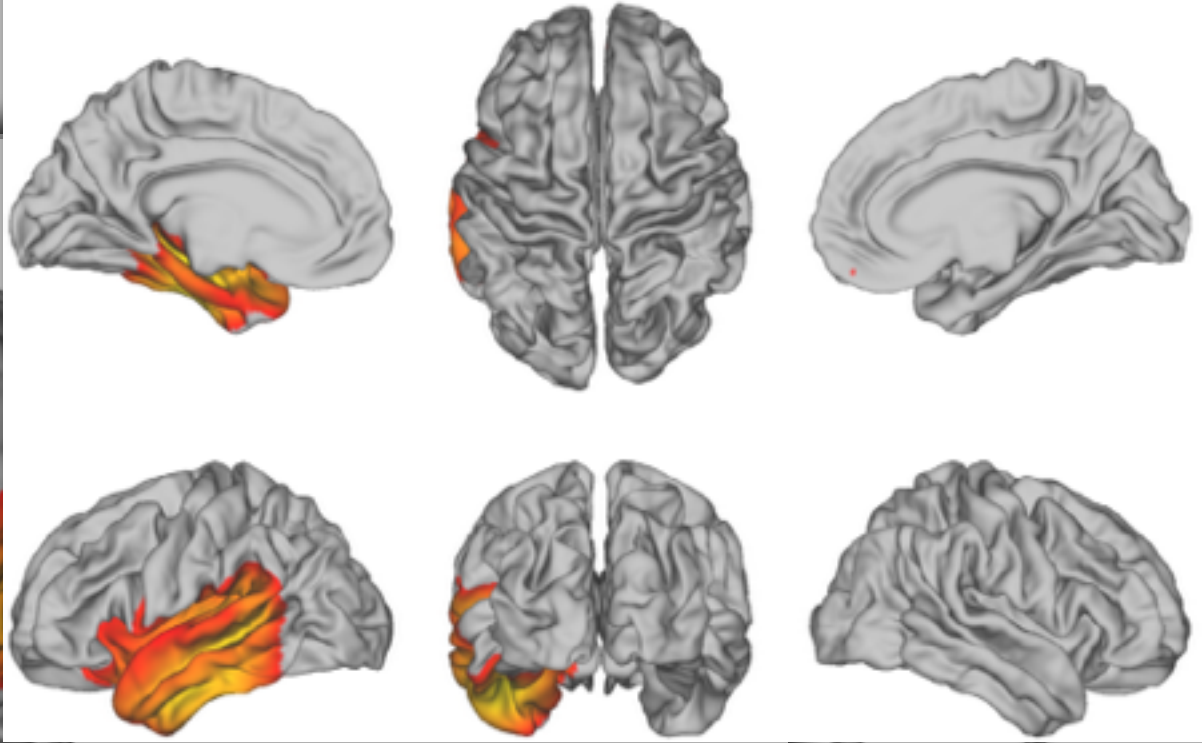
State 1  
DMN



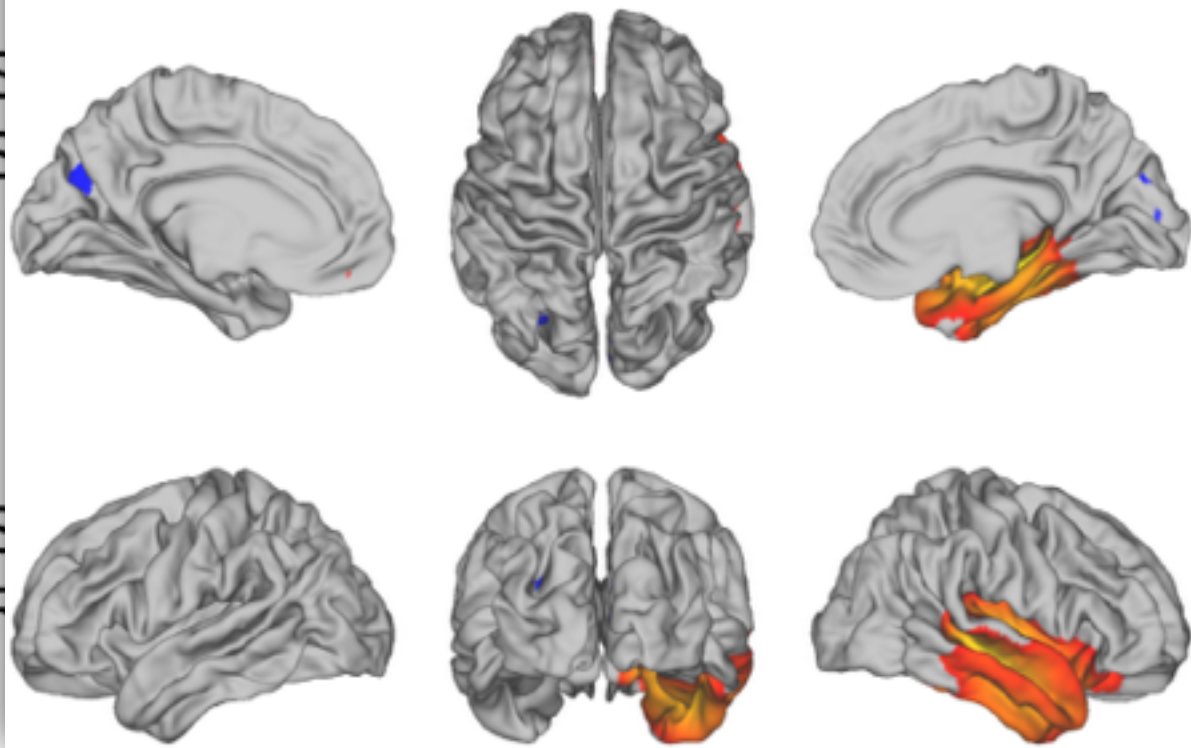
State 2  
Visual



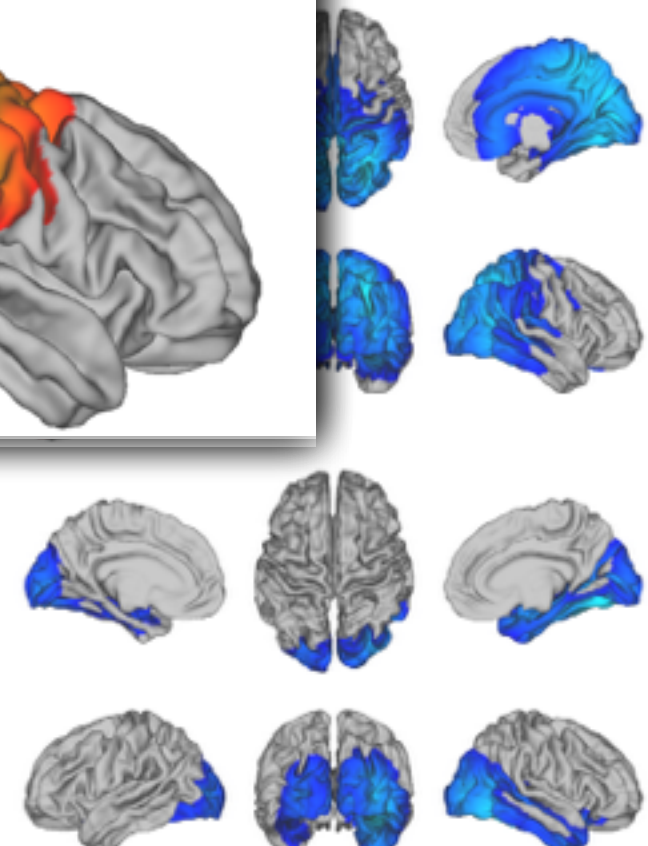
### State 5



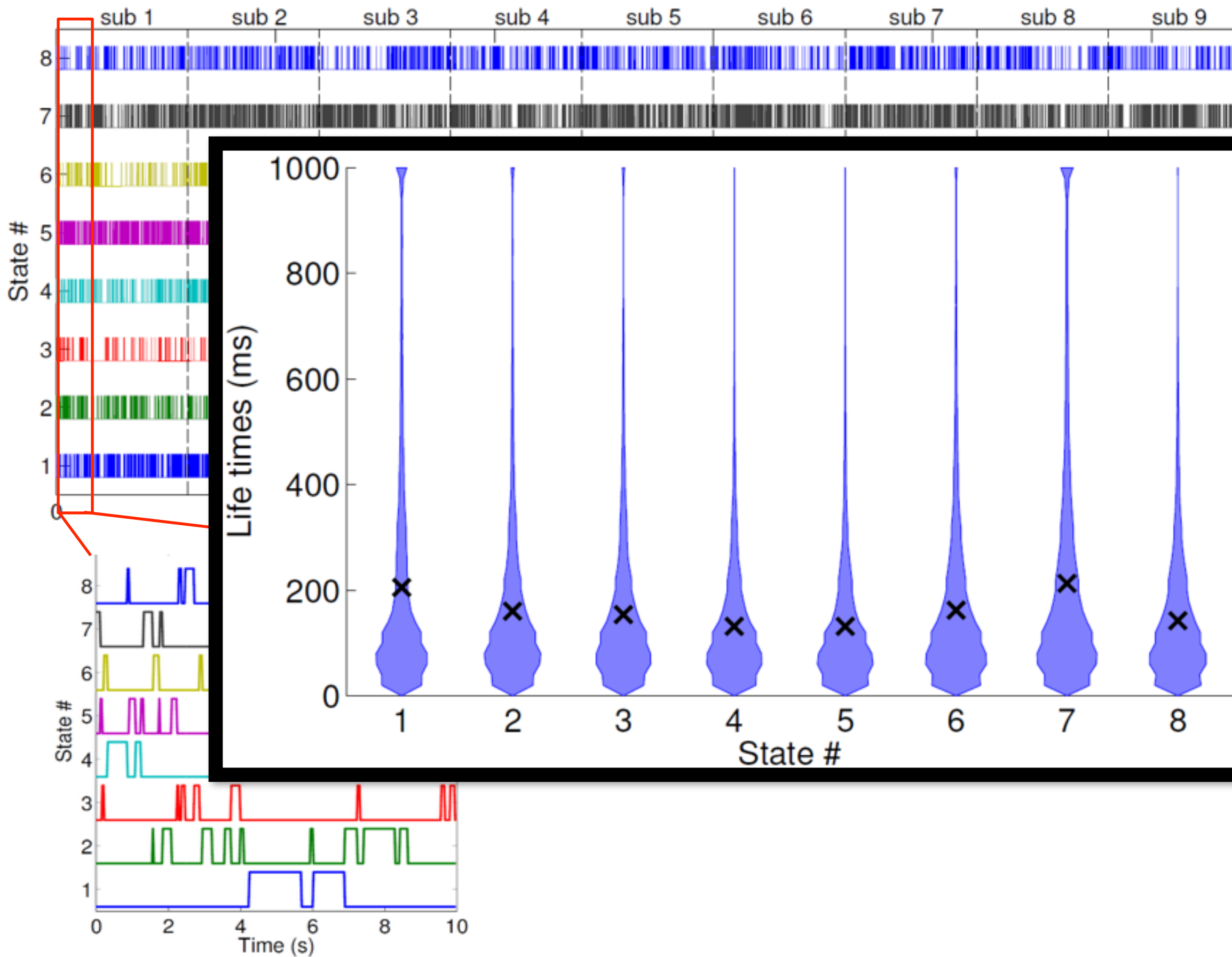
### State 4



State 8  
Visual



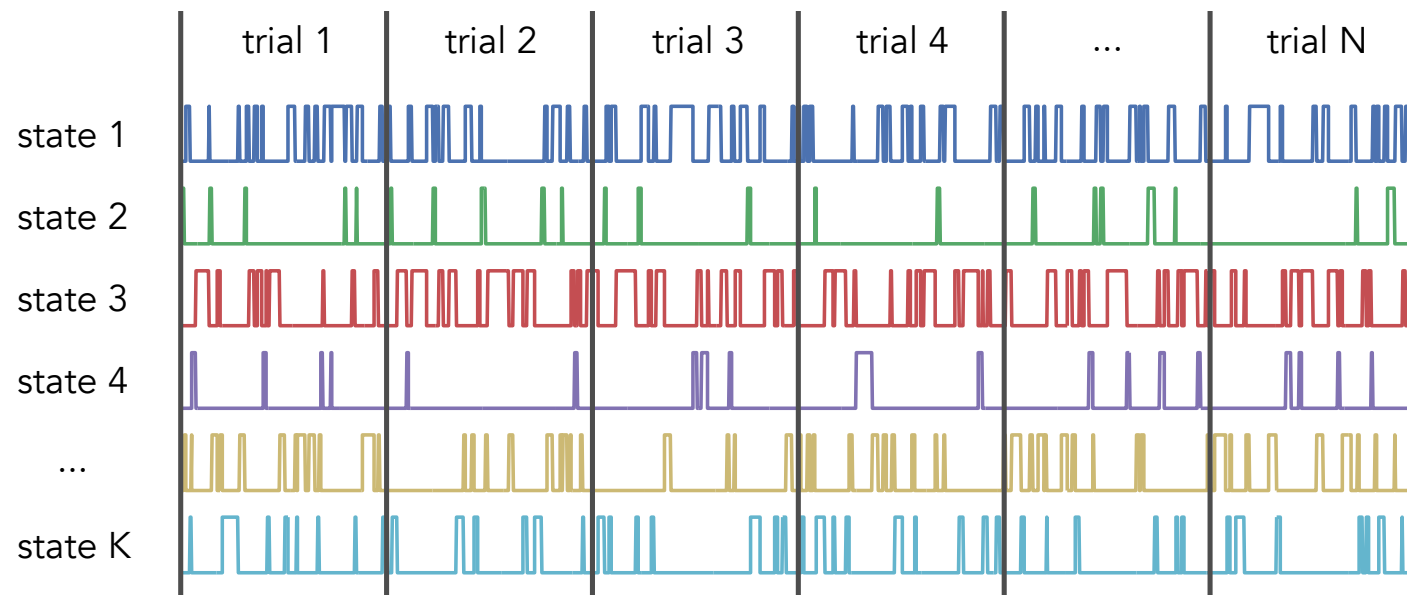
# HMM-Gaussian



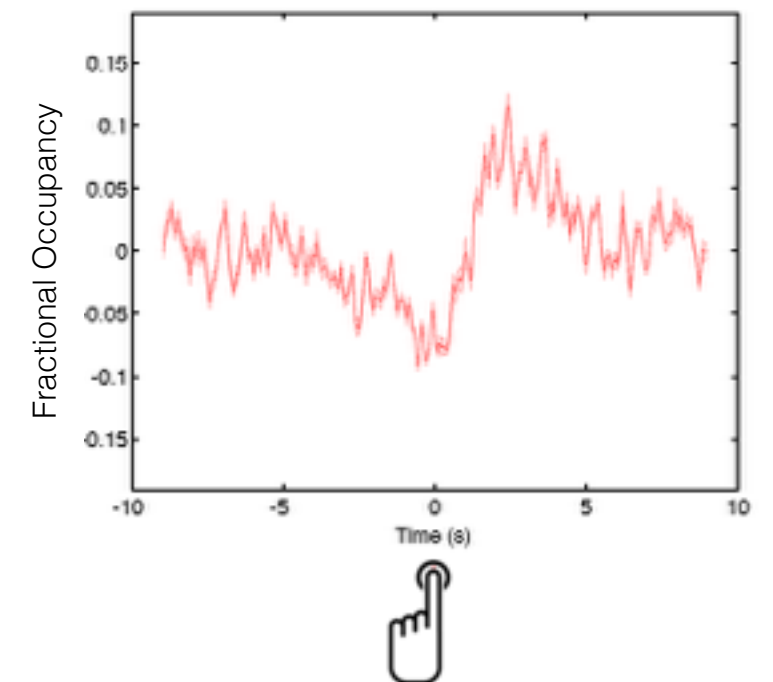
## TASK DATA

- Fit HMM to task data, **then** epoch and average the state time courses over trials

### HMM state time courses

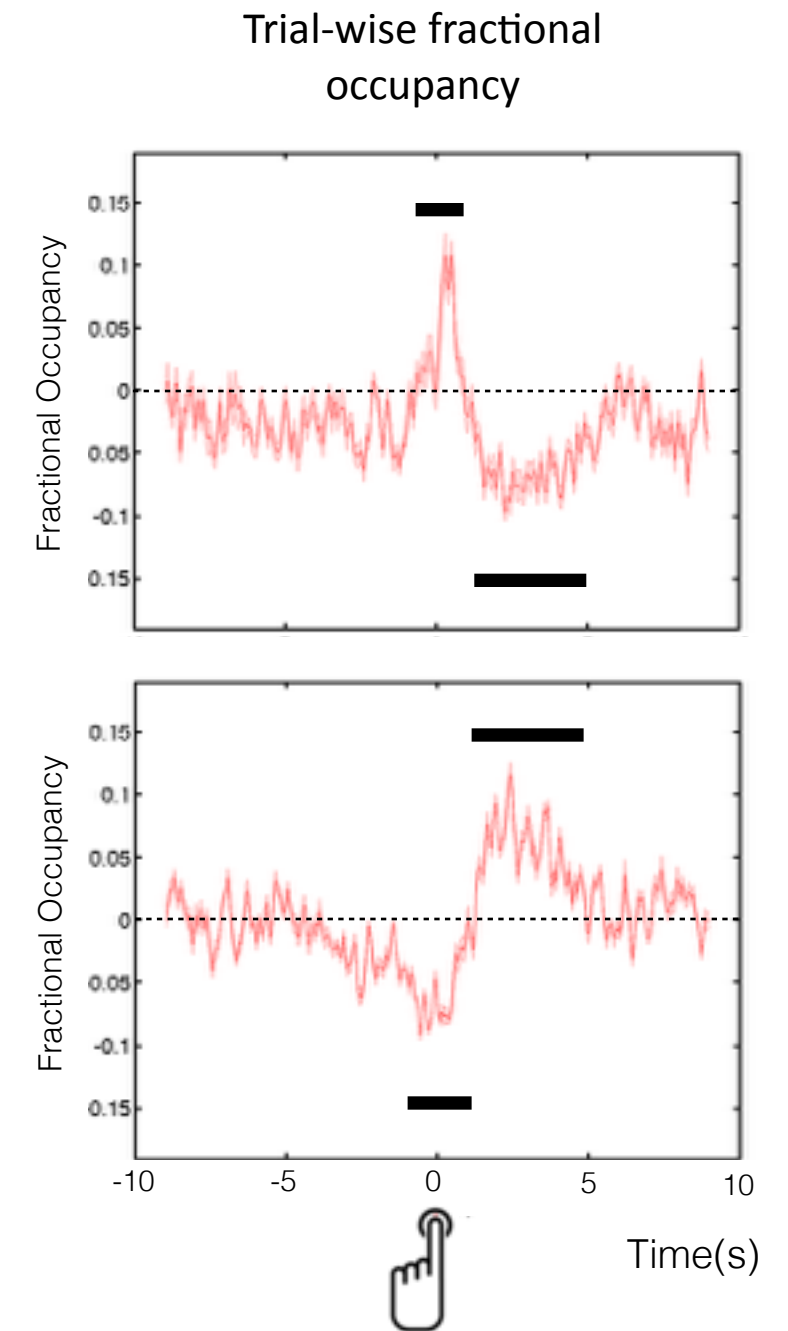
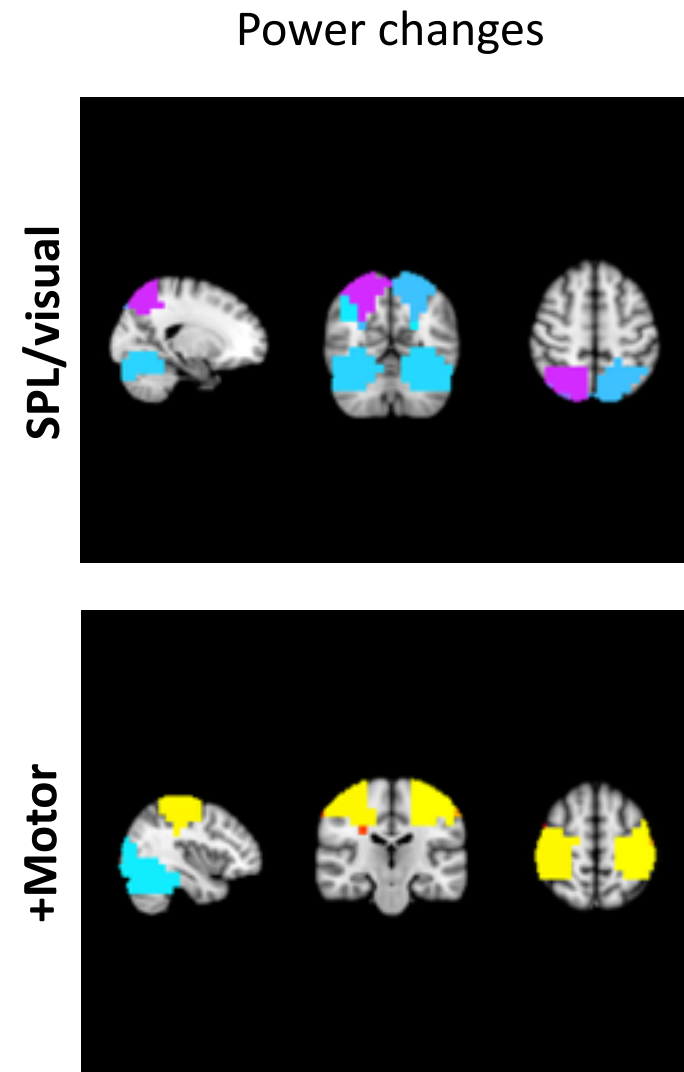


### Fractional Occupancy



- **Task-related HMM states**

- 10 subjects
- 4-30Hz
- 8 HMM states

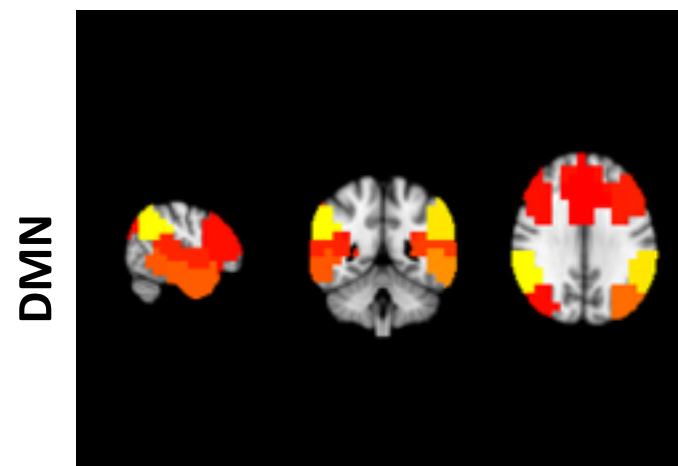
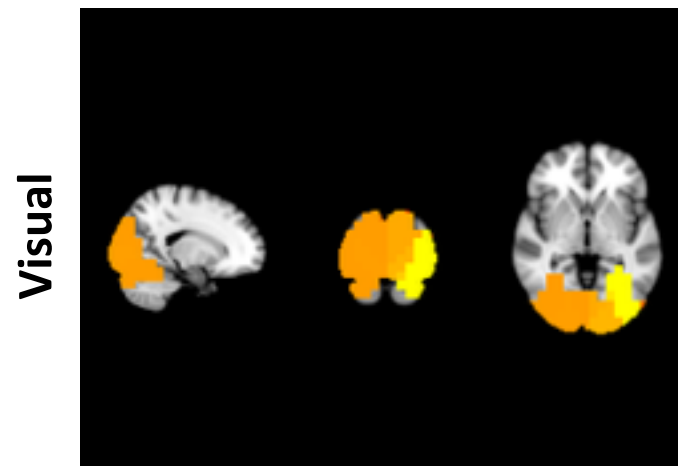




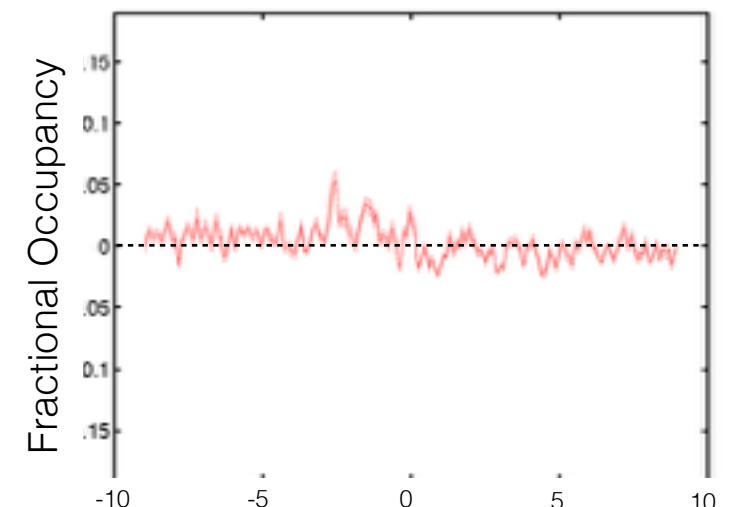
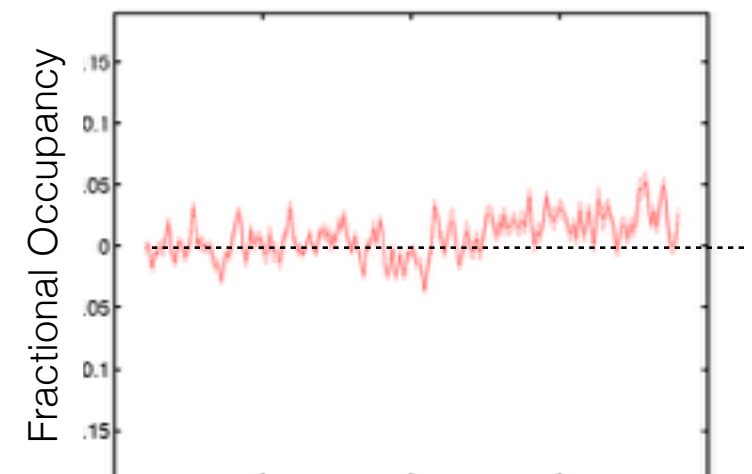
- **Task-unrelated HMM states**

- 10 subjects
- 4-30Hz
- 8 HMM states

Power changes



Trial-wise fractional occupancy



Time(s)

To set an HMM-Gaussian:

- > options = struct();
- > options.K = 8;
- > options.order = 0;
- > options.zeromean = 0;
- > options.covtype='full';
- > [hmm, Gamma] = hmmmar(X, T, options);

**No. of states**

**Model the mean**

**Full connectivity**

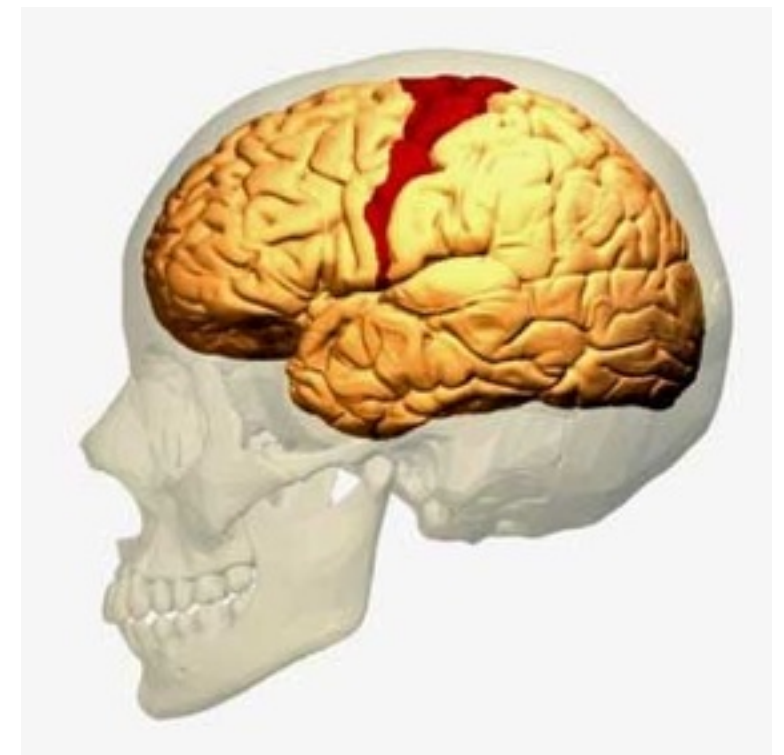
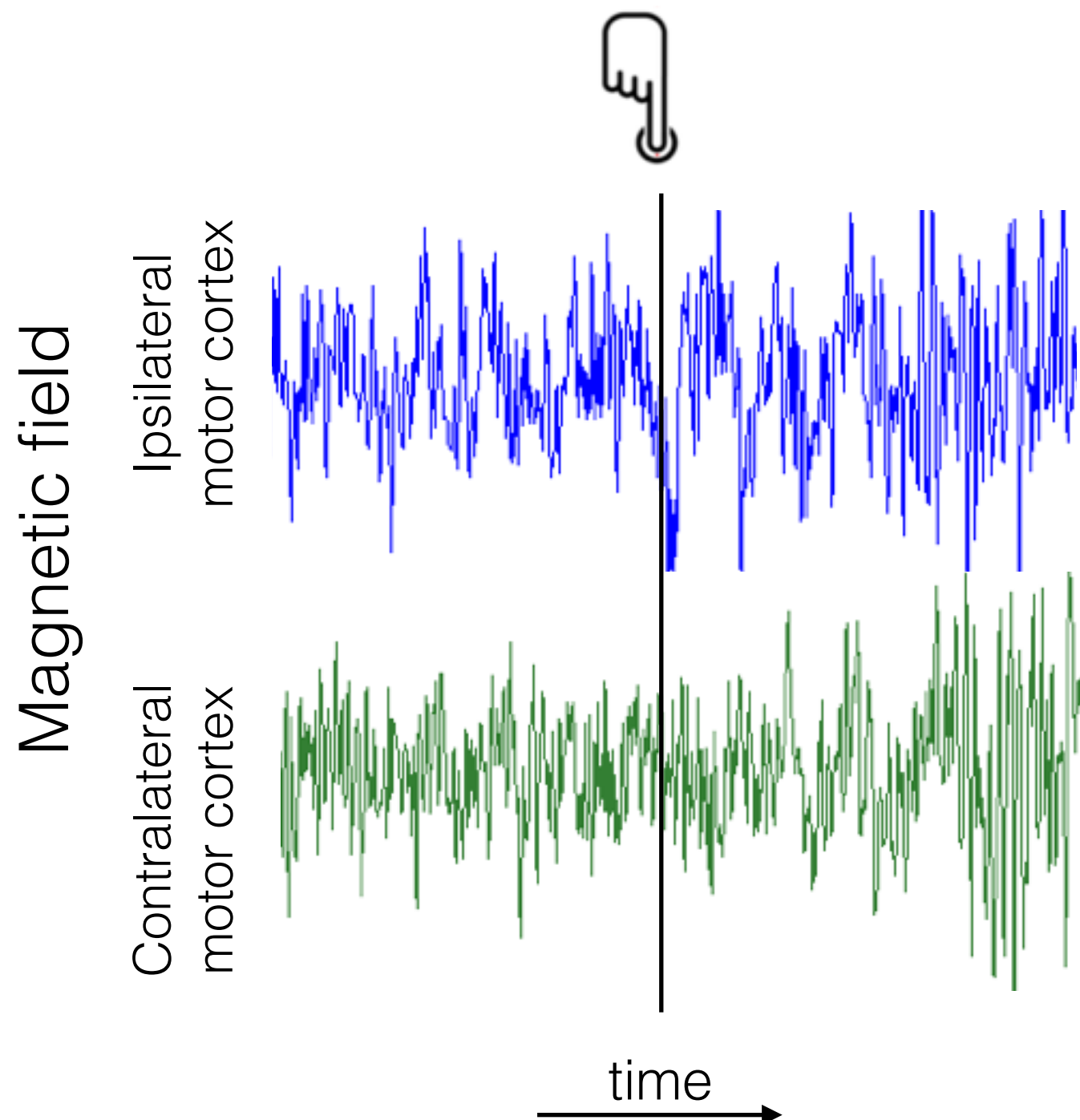
**HMM structure**

**State time courses**

In summary:

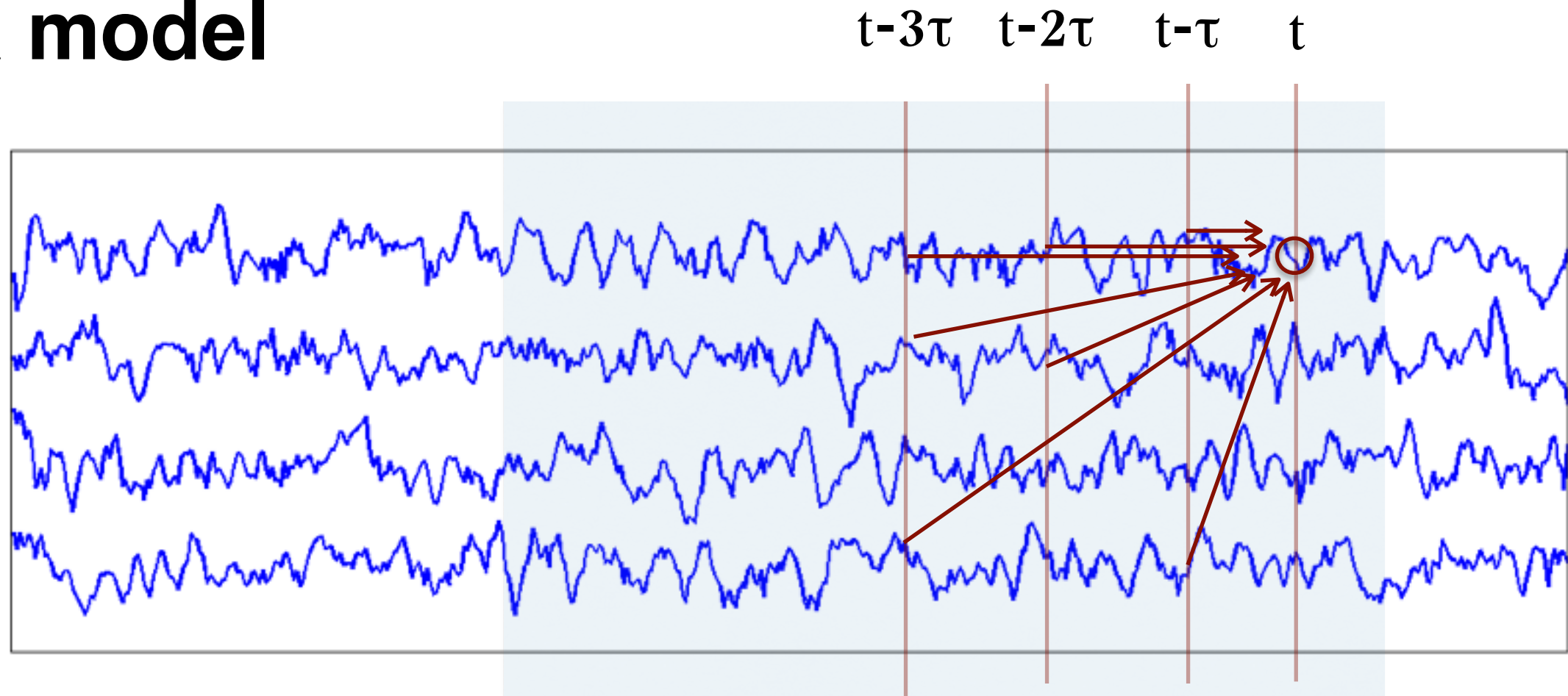
- The *HMM-Gaussian* focuses on **power** and **can be applied to whole brain**
- But: is insensitive to phase and is not frequency-resolved

what about working with raw time courses?  
e.g. can we then find time-varying phase locking?

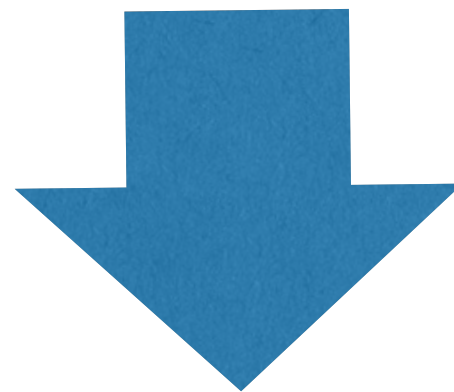




## MAR model



**Contains**

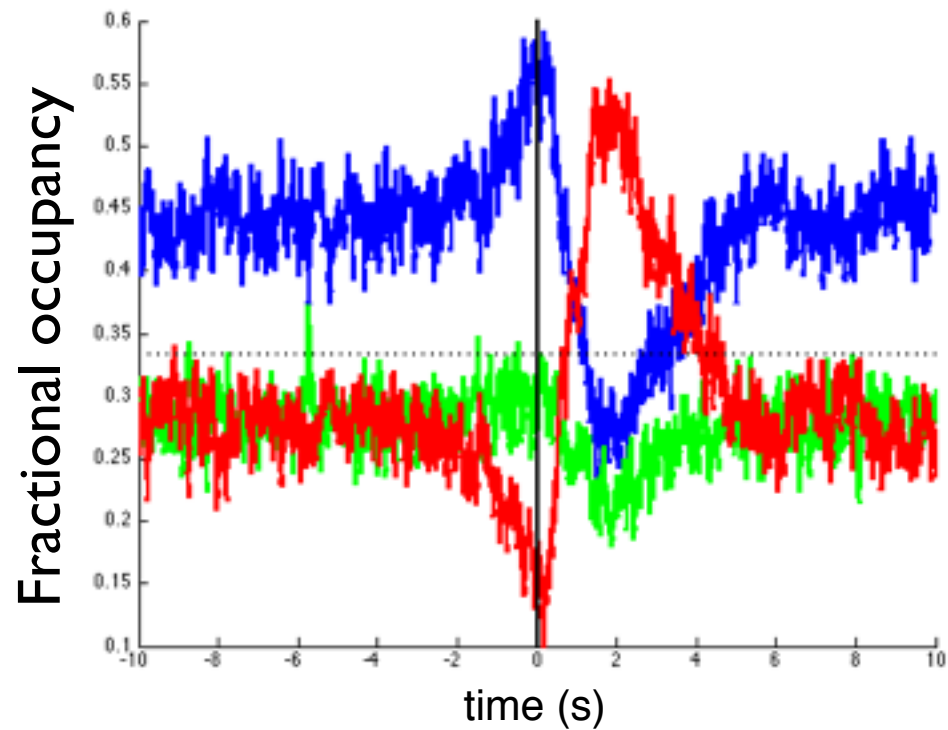


- Power spectral density
- Coherence
- Directed coherence
- Phase

## MAR model

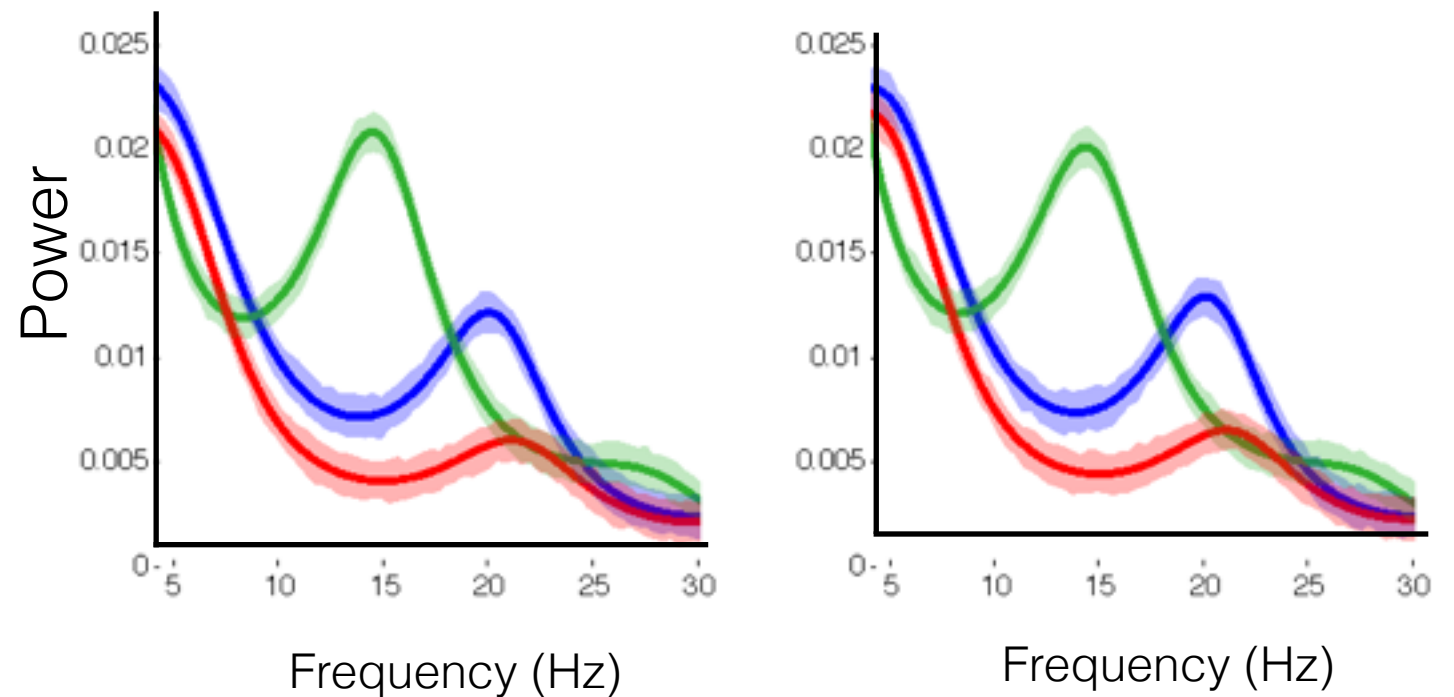
- The MAR contains information about **phase**
- It is **spectrally resolved**, i.e. all of these quantities (power, coherence, phase relations) are defined as a function of frequency

## HMM state time-courses



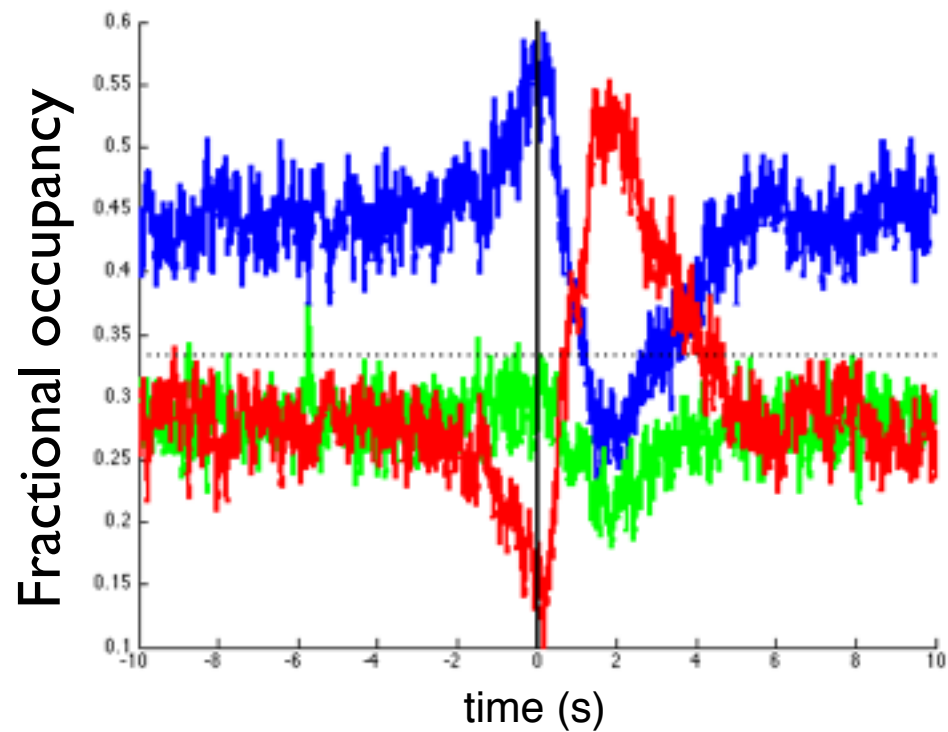
Finger-tap (beta suppression)  
 Post-finger-tap (beta rebound)  
 Baseline

## Spectral properties of each HMM state



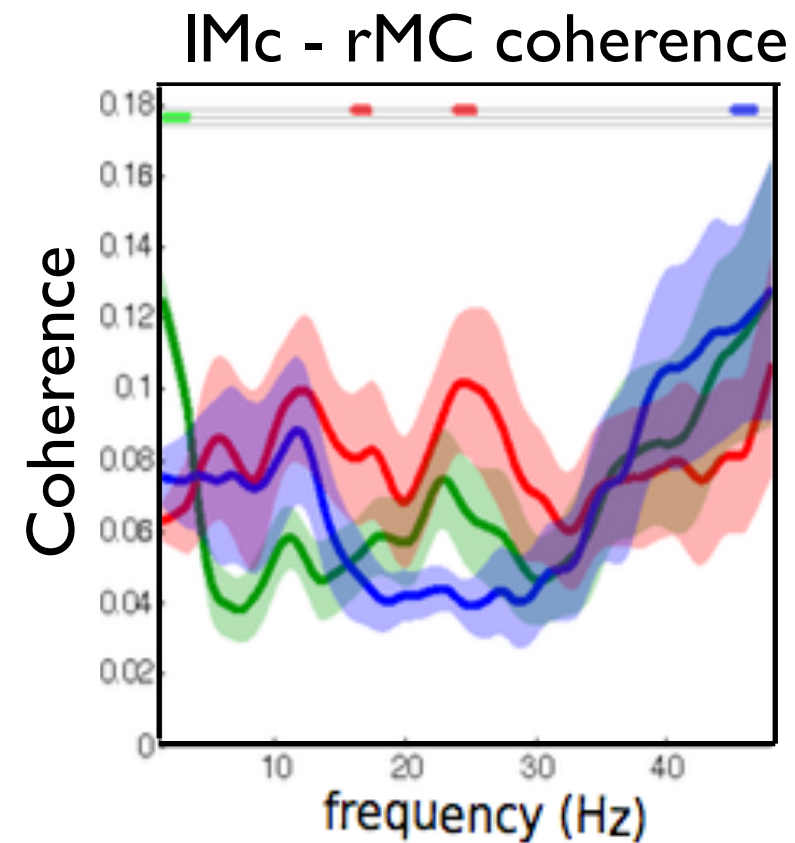
- significant state-dependent (time-varying)  
 power spectra

## HMM state time-courses



Finger-tap (beta suppression)  
 Post-finger-tap (beta rebound)  
 Baseline

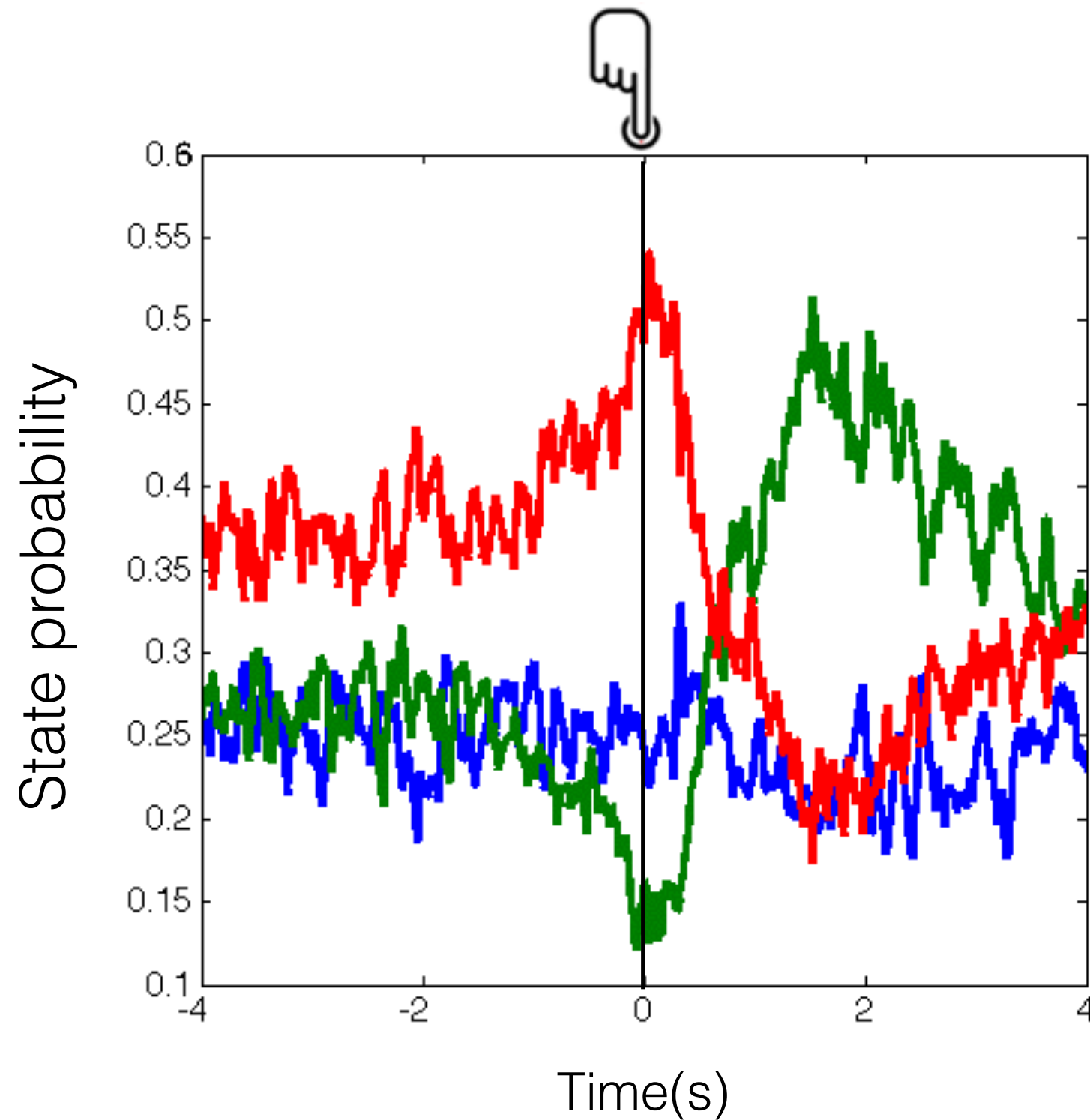
## Cross-Spectral properties of each HMM state



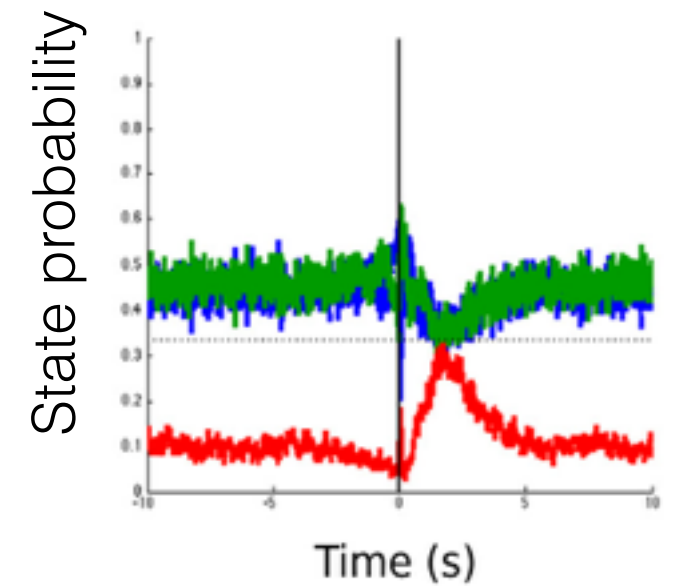
- significant state dependent (time-varying)  
 coherence (phase locking)



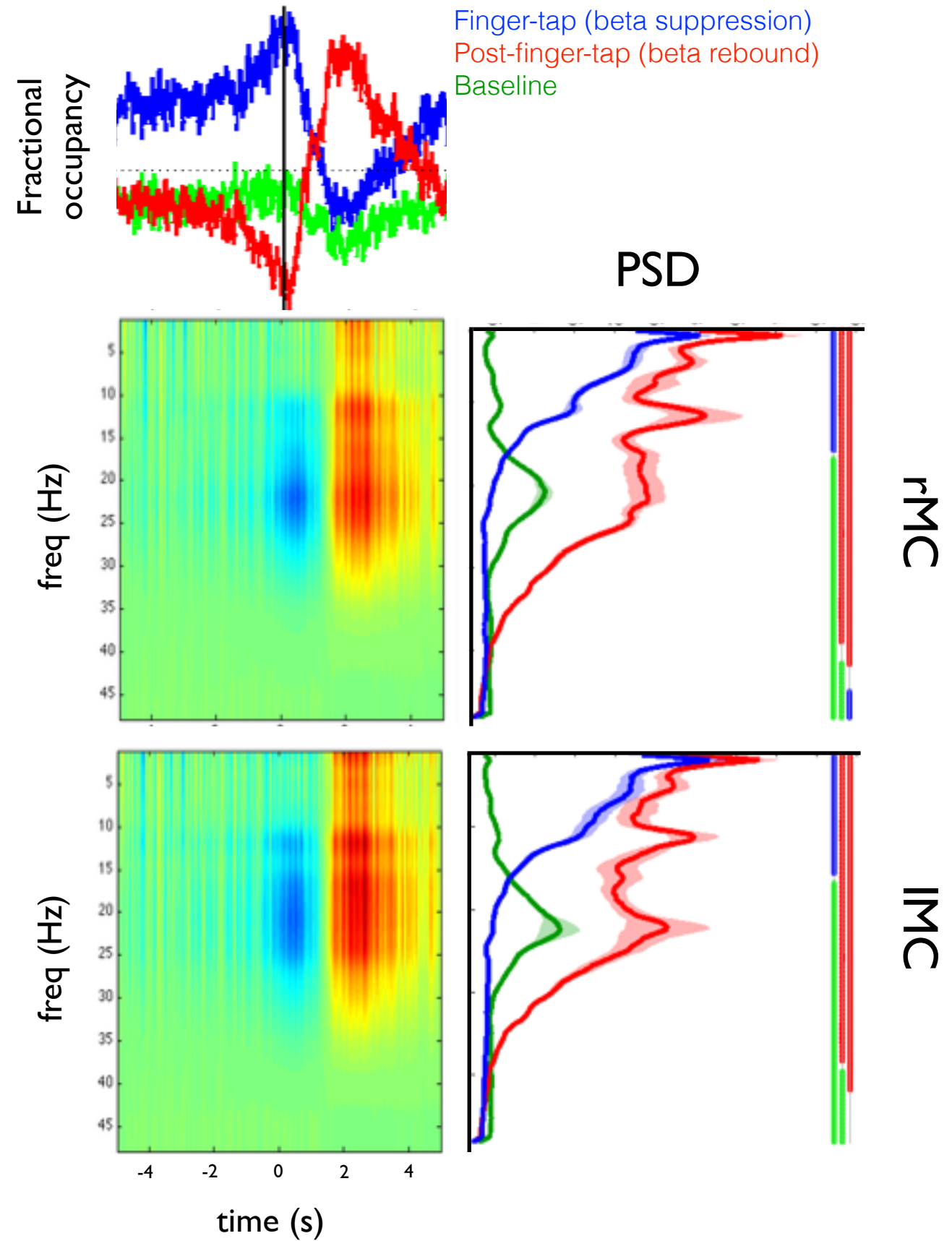
## HMM-MAR

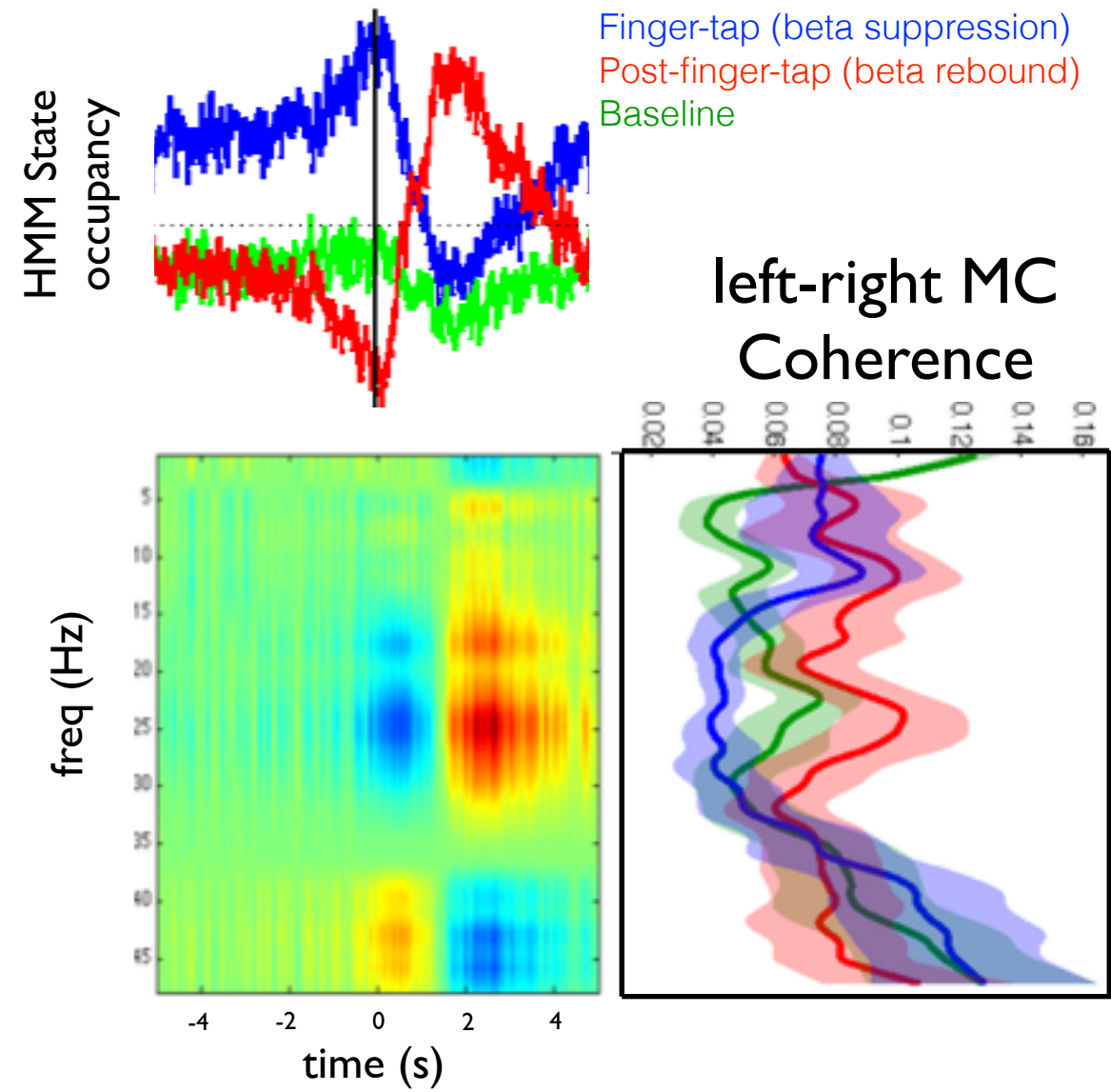


## HMM-Gaussian

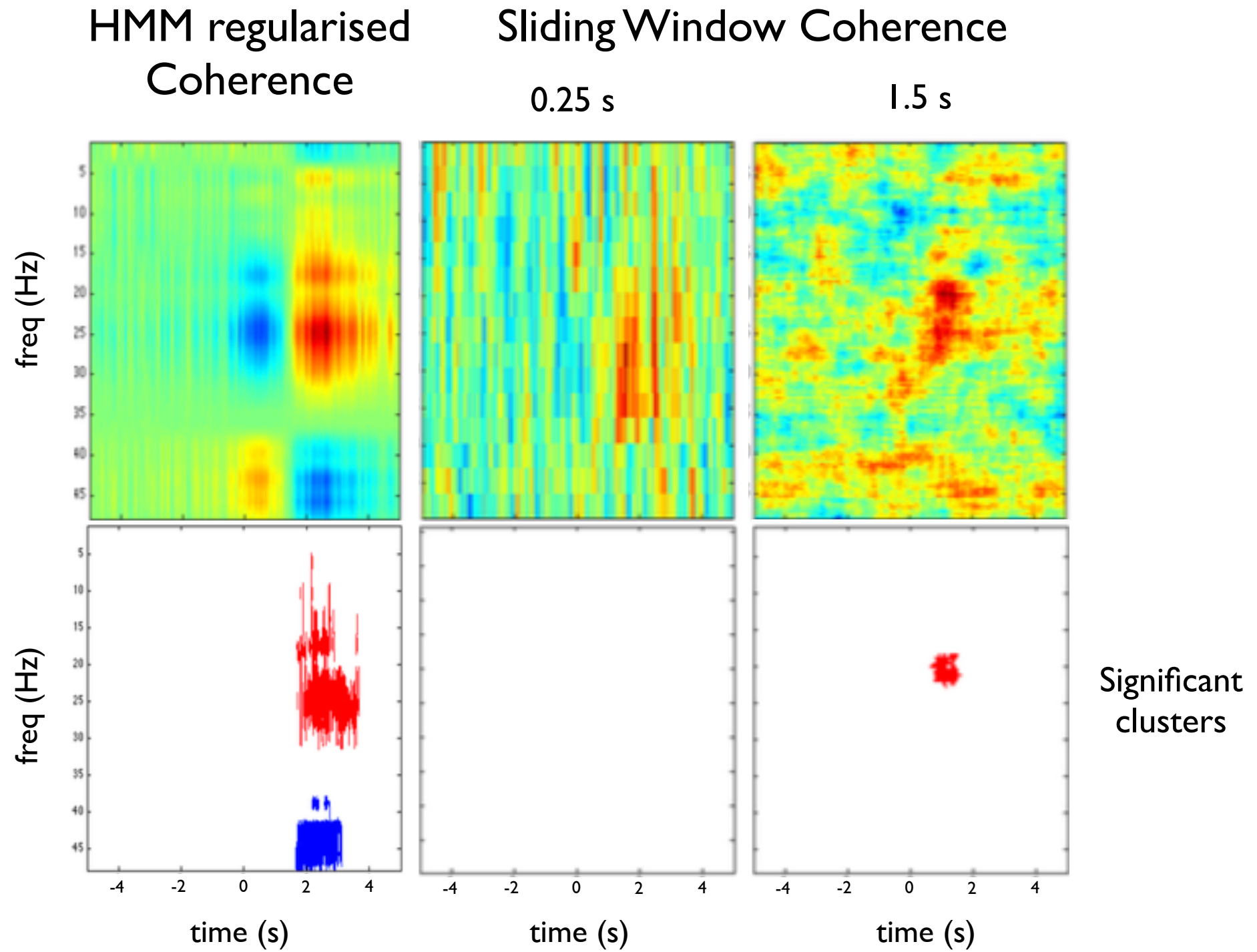


## Computing T-F Maps from HMM





HMM regularise  
Coherence





To set an HMM-MAR:

- > options = struct();
- > options.K = 3;
- > options.order = 5;
- > options.zeromean = 1;
- > options.covtype='diag';
- > [hmm, Gamma] = hmmpmar(X, T, options);

**No. of states**

**MAR order**

**HMM structure**

**State time courses**

In summary:

- The *HMM-Gaussian* approach focuses on power and **can be applied to whole brain**
- The *HMM-MAR* works on the raw time series and **is sensitive to phase information**, and is applicable to low-to-medium number of regions

More info in : <https://github.com/OHBA-analysis/HMM-MAR/wiki>

In the practicals

1. We will apply the *HMM-Gaussian* on resting state whole brain MEG data and find resting state networks that are defined in terms of activation and functional connectivity (power correlation)
2. We will apply the *HMM-MAR* on two motor regions to capture quick changes elicited during a motor task, in terms of power changes and phase coupling